

# 1 Dynamic cortical routing mediates temporal attention

2 Jiating Zhu<sup>1\*</sup>, Karen J. Tian<sup>1,2</sup>, Marisa Carrasco<sup>2</sup>, Rachel N. Denison<sup>1,2</sup>

<sup>1</sup>Psychological and Brain Science Department, Boston University, USA

<sup>2</sup>Department of Psychology and Center for Neural Science, New York University, USA

\*To whom correspondence should be addressed; E-mail: [jtszhu@bu.edu](mailto:jtszhu@bu.edu).

## 3 Abstract

4 Selecting information from dynamic streams requires mechanisms that prioritize a vi-  
5 sual stimulus at a specific moment over preceding and subsequent stimuli at the same lo-  
6 cation. Whereas selective temporal attention has been found to enhance neural responses  
7 to stimuli, its impact on communication between brain regions remains unexplored. Here,  
8 we investigated whether prioritizing a stimulus at a specific time is achieved through selec-  
9 tive routing of stimulus information across cortical networks using MEG. We developed a  
10 dynamic informational connectivity approach to quantify shared stimulus information be-  
11 tween each region and the rest of the network. When stimuli compete in time, we found that  
12 temporal attention modulated the network at both early and late post-target time windows,  
13 routing information along two possible pathways—occipito-fronto-cingulate and occipito-  
14 temporal—via both transient bursts of network communication and theta-rhythmic replay.  
15 These results provide evidence that under dynamic sensory input, the timing of neural com-  
16 munication determines stimulus selection.

## 17 Introduction

18 Sensory information is continuous and dynamic, yet the capacity to process such information  
19 is limited. To manage these constraints, humans use attention to prioritize information most  
20 relevant to their current task. For example, when caring for a baby, it is critical to prioritize parts  
21 of the visual stream that signal imminent risk—such as the baby’s hand moving toward a small  
22 object. Flexible attentional prioritization enables relevant information to guide goal-directed

23 behavior, like moving the object out of the baby's reach (Carrasco, 2011; Anton-Erxleben and  
24 Carrasco, 2013; Nobre and Van Ede, 2023; Denison, 2024).

25 Attention is thought to prioritize task-relevant information via selective routing: the prefer-  
26 ential communication across cortical networks of some stimulus information at the expense of  
27 other information. Attention enhances sensory responses to task-relevant stimuli (van Es et al.,  
28 2018; Dugué et al., 2020; Liu et al., 2021; Maunsell and Treue, 2006; Liu et al., 2007; Foster and  
29 Ling, 2022), potentially increasing the likelihood that the associated information is transmitted  
30 downstream. Attention also directly increases inter-areal communication by synchronizing neu-  
31 ronal activity across areas, such that spikes in an upstream area are more effectively transmitted  
32 to a downstream area (Fries, 2015; Salinas and Sejnowski, 2001). However, our understanding  
33 of selective routing remains limited in several respects. First, selective routing has mainly been  
34 inferred from synchronized neuronal oscillations (Banaie Boroujeni et al., 2025; Fries, 2015;  
35 Saalman et al., 2012; Womelsdorf et al., 2007), rather than by directly measuring the trans-  
36 mission of stimulus-specific information content (Van Ede et al., 2018; Kok et al., 2012; Stokes  
37 et al., 2015). Second, attentional modulation of inter-areal communication has largely been ex-  
38 amined in selected pairs of brain regions (Fries, 2015; Gregoriou et al., 2009; Buschman and  
39 Miller, 2007; Saalman et al., 2007), so little is known about how attention modulates routing  
40 across large-scale cortical networks (Banaie Boroujeni et al., 2025; Siegel et al., 2015). Third,  
41 selective routing has mainly been studied in the context of spatial attention (Fries, 2015; Bosman  
42 et al., 2012; Gregoriou et al., 2009; Buschman and Miller, 2007; Saalman et al., 2007), whereas  
43 how temporal attention affects selective routing has not been investigated. Fourth, how selec-  
44 tive routing unfolds over time for dynamic input has rarely been studied. Here we addressed  
45 these four limitations to advance understanding of how attention facilitates selective routing in  
46 dynamic settings.

47 Temporal attention refers to the prioritization of sensory information at specific points in

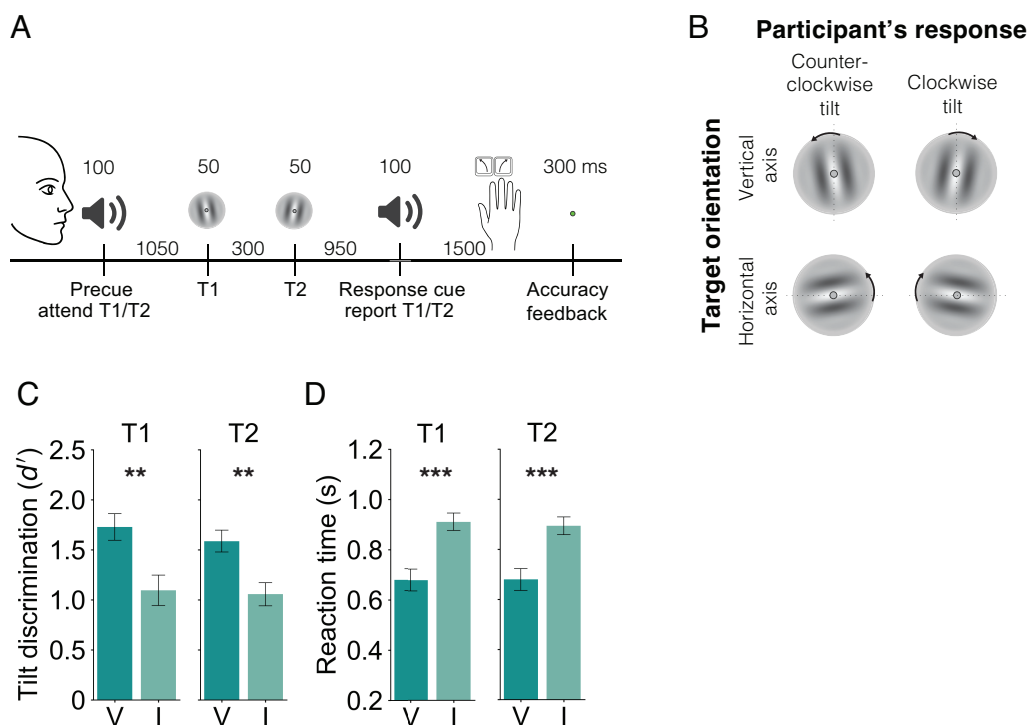
48 time, which improves perception and behavior at attended moments (Denison et al., 2017, 2021;  
49 Fernández et al., 2019; Duyar et al., 2023, 2024; Palmieri and Carrasco, 2024; Denison et al.,  
50 2024; Tian et al., 2026; Jing et al., 2023; Huang et al., 2025). For example, returning to the  
51 caregiving scenario, by anticipating when the baby might grasp a dangerous object, the care-  
52 giver can attend at the critical moment to monitor the baby’s hand position and intervene if  
53 necessary. Attending too early or too late would make it difficult to respond appropriately.  
54 Temporal orienting increases neural responses to stimuli appearing at attended moments (Cor-  
55 rea et al., 2006; Doherty et al., 2005), yet it poses a challenge for cortical routing mechanisms  
56 identified for spatial attention, which prioritizes the selective processing of one location over  
57 others presented at the same time. Spatial routing mechanisms exploit spatiotopic organization  
58 by facilitating communication along spatially specific routes, in effect selecting one of multiple  
59 routes for preferential transmission. Temporal attention, however, can prioritize stimuli pre-  
60 sented at the same spatial location but at different moments. Selective routing in the temporal  
61 domain therefore cannot rely on separate cortical populations or communication routes. In-  
62 stead, we hypothesized that temporal attention flexibly shapes the dynamics of selective routing  
63 over a shared network pathway.

64 To investigate whether and how temporal attention alters selective routing across large-scale  
65 cortical networks, we developed an analysis approach called “dynamic informational connec-  
66 tivity.” This approach is based on the informational connectivity method, which quantifies  
67 correlated fluctuations in multivariate pattern discriminability across regions (Coutanche and  
68 Thompson-Schill, 2013), thereby directly measuring shared fluctuations in stimulus-specific  
69 content across brain regions. Whereas previous studies have typically calculated a single con-  
70 nectivity estimate from extended functional magnetic resonance imaging (fMRI) time series  
71 (Coutanche and Thompson-Schill, 2013; Anzellotti and Coutanche, 2018; Huang et al., 2024;  
72 Mill and Cole, 2025), here we leveraged the high temporal resolution of magnetoencephalog-

73 raphy (MEG) and sliding time windows to capture rapid fluctuations in informational connec-  
74 tivity. To quantify informational connectivity across large-scale networks, we combined this  
75 approach with graph-theory metrics.

76 We recorded MEG while human participants performed a temporal attention task, in which  
77 they were instructed to attend to one of two consecutive target stimuli presented at the same  
78 spatial location, with one target more likely to be task relevant. We used source-reconstruction  
79 to estimate neural activity across large-scale cortical networks during this task. To track the flow  
80 of stimulus information—and to overcome the challenge that successive stimuli may engage  
81 overlapping neural populations—we independently decoded the identity of each stimulus and  
82 quantified how decoding accuracy, as a measure of stimulus information, was shared across  
83 areas and networks in a time-resolved fashion.

84 Our results revealed that temporal attention alters informational connectivity across large-  
85 scale cortical networks. Temporal attention led to discrete, stimulus-specific bursts of increased  
86 connectivity at both early and late time windows during the trial, indicating that selective rout-  
87 ing is neither instantaneous nor sustained continuously. The connectivity changes coalesced  
88 along two principal pathways—an occipital-temporal route and an occipital-fronto-cingulate  
89 route—which appeared to play different roles in maintaining stimulus information throughout  
90 the trial and mediating the transition from processing the first to the second target, respectively.  
91 Finally, we observed a periodic recurrence at 4 Hz of occipital decoding patterns within the  
92 temporal lobe following both targets. Altogether, these findings reveal how temporal attention  
93 dynamically and selectively routes stimulus information across large-scale cortical networks in  
94 the service of flexible behavior.



**Figure 1.** Two-target temporal cueing task. **(A)** Trial timeline showing stimulus durations and SOAs. Precues and response cues were pure tones (high = cue T1, low = cue T2). **(B)** Each target was independently tilted along either the vertical or horizontal axis. Participants reported whether the target specified by the response cue was tilted clockwise or counterclockwise, while the axis orientation served as the stimulus feature decoded in the analysis. **(C)** Tilt discrimination (sensitivity) and **(D)** reaction time for each target (T1, T2) by validity condition. Results are previously reported in (Zhu et al., 2024). Sensitivity was higher and reaction time was faster for valid (V) than invalid (I) trials. Error bars indicate  $\pm 1$  SEM. \*\*  $p < 0.01$ ; \*\*\*  $p < 0.001$ .

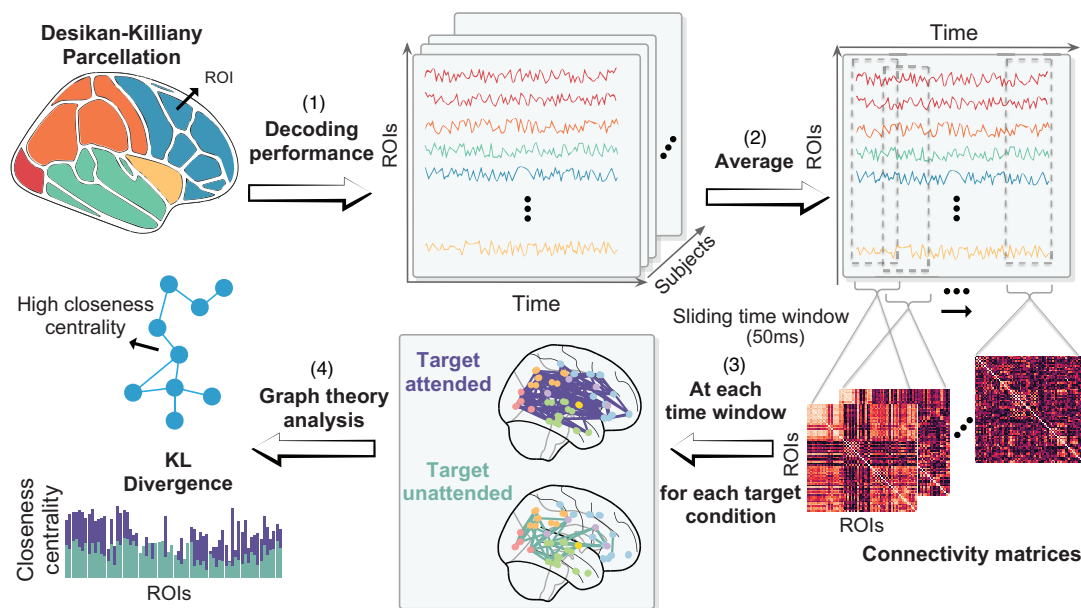
## 95 **Results**

### 96 **Temporal attention improved orientation discrimination**

97 Participants performed a two-target temporal cueing task while MEG was recorded (**Figure 1A**).  
98 Each trial presented two sequential gratings separated by a 300 ms stimulus onset asynchrony.  
99 A precue tone at the start of the trial instructed participants to attend to either the first (T1) or  
100 the second (T2) target, and a response cue at the end of the trial indicated which target's tilt  
101 should be reported. Participants reported whether the tilt of the indicated target was clockwise  
102 or counterclockwise relative to the vertical or horizontal axis (**Figure 1B**). On 75% of trials the  
103 precue and response cue matched (valid) and on 25% they mismatched (invalid), incentivizing  
104 participants to prioritize the precued target. Gratings were tilted independently around either the  
105 vertical or horizontal axis, enabling MEG decoding of axis orientation—a feature orthogonal  
106 to the participant's report. Temporal attention improved tilt discriminability (**Figure 1C**; main  
107 effect of validity:  $F(1, 9) = 20.22$ ,  $p = 0.0015$ ,  $\eta_G^2 = 0.25$ ) and response times (**Figure 1D**;  
108 main effect of validity:  $F(1, 9) = 70.60$ ,  $p < 0.001$ ,  $\eta_G^2 = 0.32$ ) for both targets. Full behavioral  
109 results were reported in (Zhu et al., 2024); see also **Supplementary Figure 1**.

### 110 **Dynamic informational connectivity analysis**

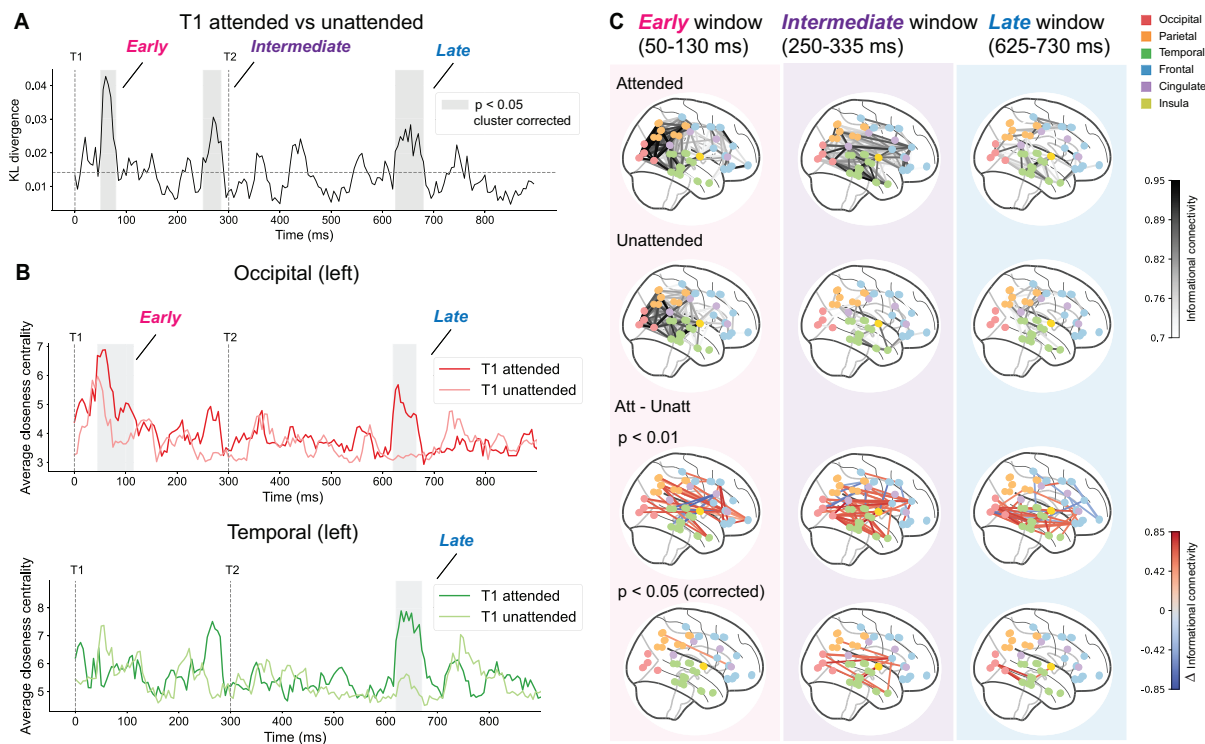
111 To investigate the flow of stimulus information across the cortex, we used informational con-  
112 nectivity (Coutanche and Thompson-Schill, 2013; Anzellotti and Coutanche, 2018) to measure  
113 shared fluctuations in stimulus information across brain regions. For each atlas-based brain  
114 region (34 per hemisphere, (Desikan et al., 2006), **Supplementary Table 1**) from MEG source-  
115 reconstructed data, and for each target separately, we decoded stimulus orientation (vertical vs.  
116 horizontal) from the multivariate neural activity pattern with 5-ms resolution. Then we calcu-  
117 lated the correlation between the decoding accuracy time series from each pair of regions in  
118 the cortex. We used a 50-ms sliding time window to estimate informational connectivity in a



**Figure 2.** Whole-brain comparison of informational connectivity between target-attended and target-unattended conditions. (1) For each region, we trained an SVM classifier to decode target axis orientation from source-reconstructed MEG data in a time-resolved fashion. (2) Decoding accuracy for each region was averaged across subjects. (3) For each target condition, we then computed the correlation of decoding accuracy (edges) across all pairs of atlas-based regions (nodes) within sliding time windows. (4) At each time window, closeness centrality for each region was defined as the average inverse correlation distance to all other regions. This yielded a distribution of closeness centrality across all regions. Finally, we compared the spatial patterns of closeness centrality between conditions using Kullback–Leibler (KL) divergence.

119 time-resolved fashion across the trial, yielding a dynamic informational connectivity analysis  
120 (**Figure 2**). This procedure, applied to all pairs of brain regions, produced an informational  
121 connectivity network for each target (T1 or T2), time window, and attention condition (tar-  
122 get attended or unattended). For subsequent graph theory analyses on these networks, each  
123 atlas-based region was considered a node, and the correlation in stimulus orientation decoding  
124 accuracy for a pair of regions was considered an edge.

125 We first aimed to determine whether temporal attention altered the informational connectiv-  
126 ity network structure across time. To do so, we estimated the degree of stimulus information  
127 sharing, separately for each target, between each brain region and the rest of the network at each  
128 time step. We quantified information sharing using the graph theory property of closeness cen-  
129 trality, calculated as the average inverse correlation distance from one node to all other nodes.  
130 Regions with higher closeness centrality in a given time window thus exhibit more similar orien-  
131 tation decoding time series to other brain regions within that time window. To assess effects of  
132 attention on the network structure, we used Kullback-Leibler (KL) divergence to compare close-  
133 ness centrality distributions (across nodes) for target attended vs. unattended networks, again  
134 for each target and time window (see **Methods**, *Dynamic informational connectivity analysis*).  
135 This procedure provided a data-driven approach to assess whether attention to a target changed  
136 how stimulus information for that target was shared across the cortical network over time. This  
137 approach goes beyond assessing correlations between specific pairs of regions by summarizing  
138 the network structure of informational connectivity.



**Figure 3.** Modulation of informational connectivity for T1. Plotted time series values are indexed to the time point at the start of the sliding window used to compute the value. **(A)** KL divergence between T1 attended vs. T1 unattended informational connectivity networks indicate significant divergence at three time windows (early 50-130 ms, intermediate 250-335 ms, late 625-730 ms) from T1 onset. The horizontal dashed line marks the average value over the time window of interest (0-900 ms), as a baseline measure. Each shaded window shows the range between starting time points of the first and last sliding windows in the significant interval, whereas the range reported in text comprises the starting time point of first to the ending time point of the last sliding window in the interval. **(B)** Temporal attention enhanced average closeness centrality values for ROIs in the left occipital lobe at an early (45-165 ms) and a late (620-715 ms) time window after target onset, and in left temporal lobe in a late (620-720 ms) window. Gray shaded regions indicate cluster corrected  $p < 0.05$  (threshold were 0.85 for the early window and 0.95 for the late windows). The same shading convention as in **(A)**. **(C)** Average informational connectivity at the early, intermediate, and late time windows. The visualization of target attended networks is on the first row, and target unattended networks on the second row. Darker edges indicate stronger connectivity. The third row shows the difference in informational connectivity between attended and unattended conditions. The presented edges are significant at  $p < 0.01$  compared to a shuffled null distribution, with red edges indicating higher attended connectivity. The fourth row presents the FDR corrected edges ( $p < 0.05$ ).

## 139 **Temporal attention changed informational connectivity at both early and** 140 **late post-target time windows**

### 141 **T1 informational network**

142 The KL divergence between T1 attended and unattended networks (**Figure 3A**) showed that  
143 temporal attention changed the spatial pattern of closeness centrality in three time windows:  
144 early (50-130 ms after T1 onset,  $p = 0.04$  cluster corrected one-sided permutation test); in-  
145 termediate (250-335 ms after T1 onset  $p = 0.03$  cluster corrected), right before T2 onset; and  
146 late, 625-730 ms after T1 onset ( $\sim 300$  ms after T2 onset,  $p < 0.001$  cluster corrected). To  
147 investigate which brain areas contributed to these network differences, we obtained closeness  
148 centrality measures for the occipital, parietal, temporal, frontal, and cingulate lobes by aver-  
149 aging closeness centrality values across the atlas-based regions within each lobe within each  
150 significant time window.

151 We hypothesized that attention increases shared stimulus information across the network;  
152 thus, we expected higher closeness centrality for the attended than the unattended condition.  
153 Consistent with this prediction, we found that the average closeness centrality in the occipital  
154 lobe was enhanced in early (45-165 ms after T1 onset,  $p = 0.032$  cluster corrected) and late  
155 (620-715 ms after T1 onset,  $p = 0.038$  cluster corrected) time windows (**Figure 3B**). The av-  
156 erage closeness centrality in the temporal lobe was also enhanced during the same late window  
157 (620-720 ms after T1 onset,  $p = 0.026$  cluster corrected). These enhancements were specific  
158 to the left hemisphere. Other lobes did not exhibit significant closeness centrality changes with  
159 attention after cluster correction across the time series ( $p > 0.05$ ).

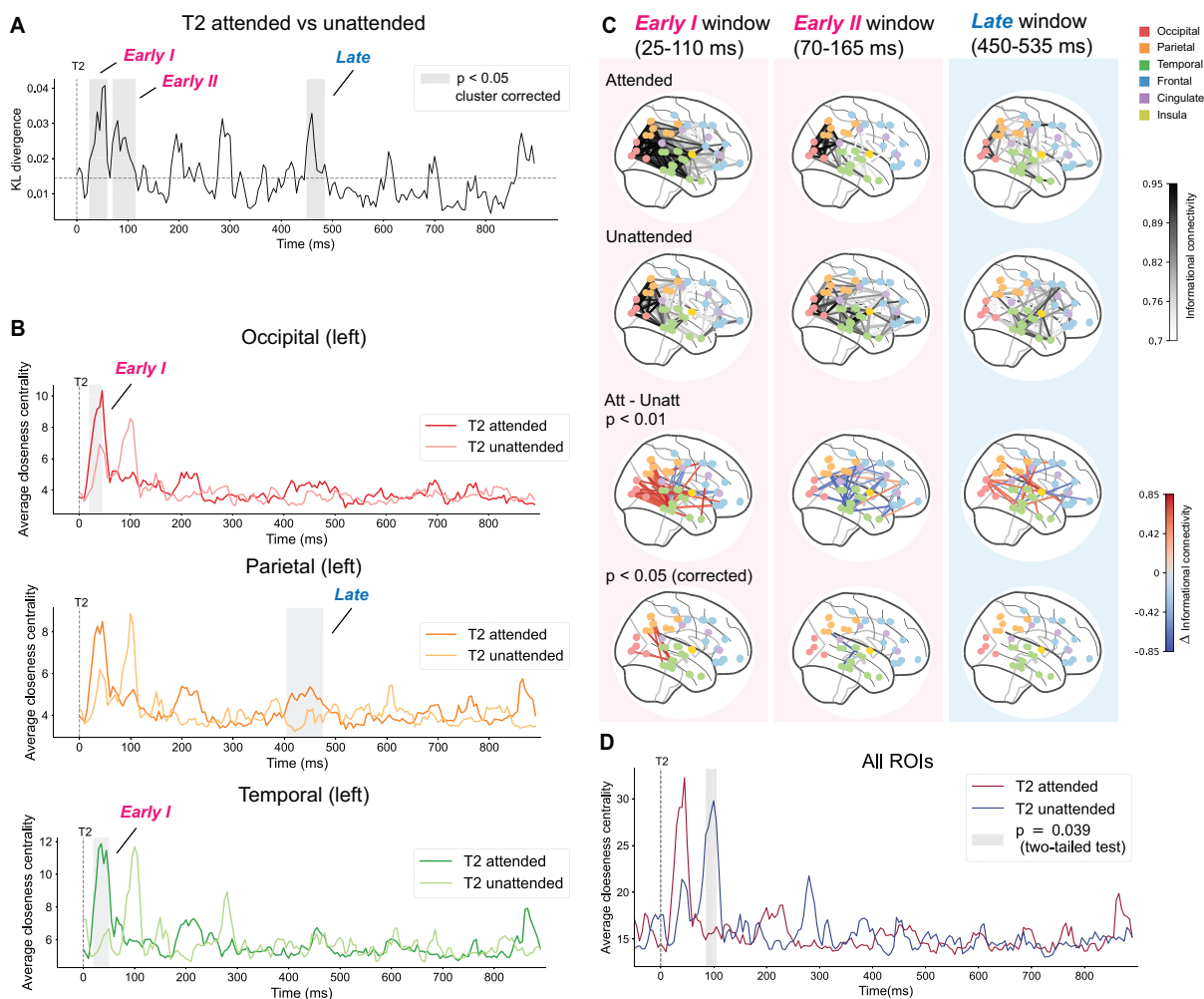
160 Closeness centrality was calculated based on decoding accuracy, so we assessed whether  
161 the observed attentional increases in closeness centrality were accompanied by corresponding  
162 changes in decoding accuracy. Although decoding accuracy increased following the target,  
163 attention did not affect decoding accuracy in either left occipital or temporal lobe (**Supple-**

164 **mentary Figure 2A**). These results indicate that the attentional changes in closeness centrality  
165 emerged at a network level, independent of local changes in decoding accuracy.

166 We next visualized the anatomical organization of informational connectivity across the  
167 network (**Figure 3C**). For each significant time window, we averaged the correlation values  
168 for each pair of nodes across all successive sliding windows (5 ms stride and 50 ms window  
169 size) contained within the significant window. Across all three time windows, the overall net-  
170 work connectivity was consistently stronger in the attended than the unattended condition. In  
171 the early time window, informational connectivity in the T1 attended and unattended networks  
172 was strongest in posterior brain areas. This pattern was expected given that stimulus informa-  
173 tion travels through the visual hierarchy starting from the occipital lobe. Occipital connectivity  
174 appeared stronger for the T1 attended than the T1 unattended network in the early time win-  
175 dow (**Figure 3C, top two rows**), consistent with the closeness centrality time series analysis  
176 (**Figure 3B**). However, few individual connectivity edges survived FDR correction for multi-  
177 ple comparisons across edges in the early time window (**Figure 3C, bottom row**). In both the  
178 intermediate and late windows, there was a strong attentional enhancement of informational  
179 connectivity between nodes in the occipital and temporal lobes, which survived FDR correction  
180 ( $p < 0.05$ ).

## 181 **T2 informational network**

182 Similar to T1, KL divergence between T2 attended and unattended networks (**Figure 4A**)  
183 showed that temporal attention changed the spatial pattern of closeness centrality at both early  
184 (“early-1”, 25-110 ms after T2 onset,  $p = 0.017$  cluster corrected; “early-2”, 70-165 ms after  
185 T2 onset,  $p = 0.003$  cluster corrected) and late time windows (450-535 ms after T2 onset,  $p$   
186  $= 0.046$  cluster corrected). Closeness centrality averaged across the regions within each lobe  
187 showed temporal attentional enhancements in the early-1 time window in the occipital (20–95



**Figure 4.** Modulation of informational connectivity for T2. **(A)** KL divergence between T2 attended vs. T2 unattended informational connectivity networks indicate significant divergence at early-1 (25-110 ms), early-2 (70-165 ms) and late (450-535 ms) time windows from T2 onset. The horizontal dashed line marks the average value over the time window of interest (0-900 ms). **(B)** Temporal attention enhanced average closeness centrality values for ROIs in the left occipital and temporal lobes at an early (20–95 ms) time window after target onset, and in the left parietal in a late (405–525 ms) window after target onset. Gray shaded regions indicate cluster corrected  $p < 0.05$  (thresholds were 0.99 for the early windows and 0.85 for the late window). **(C)** Average informational connectivity at the early-1, early-2, and late time windows. The visualization of target attended networks is on the first row, and target unattended networks on the second row. Darker edges indicate stronger connectivity. The third row shows the difference in informational connectivity between attended and unattended conditions. The presented edges are significant at  $p < 0.01$  compared to a shuffled null distribution, with red edges indicating higher attended connectivity. The fourth row presents the FDR corrected edges ( $p < 0.05$ ). **(D)** Early modulation 85–155 ms after target onset for closeness centrality averaged all ROIs in the brain for T2. The peak for T2 unattended was delayed relative to the T2 attended peak. The threshold used for cluster correction here was 0.99. Plotting conventions are the same as for **Figure 3**.

188 ms after T2 onset,  $p = 0.035$  cluster corrected) and temporal (20–100 ms after T2 onset,  $p$   
189  $= 0.013$  cluster corrected) lobes, and the late window (405–525 ms after T2 onset,  $p = 0.045$   
190 cluster corrected) in the parietal lobe (**Figure 4C**).

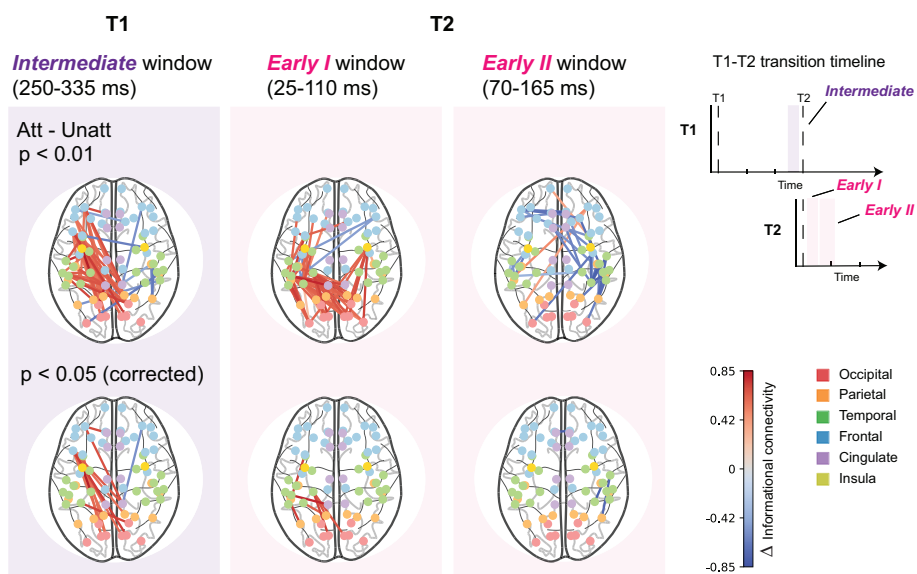
191 When T2 was unattended, the increase in closeness centrality just after the target onset  
192 appeared to be delayed in a manner that was widespread across lobes. We evaluated this ob-  
193 servation with a two-sided test on all ROIs and found that the closeness centrality of the T2  
194 unattended network was significantly enhanced in the early-2 time window (85–155 ms after  
195 T2 onset,  $p = 0.039$  cluster corrected two-sided permutation test), reflecting a delay of 60  
196 ms in the early closeness centrality peak in unattended relative to attended trials (**Figure 4D**).  
197 The early-1 attentional enhancement, in contrast, was more localized in the left occipital and  
198 temporal lobes and did not survive across all lobes.

199 The attentional increases in closeness centrality for T2 were again not accompanied by  
200 attentional changes in decoding accuracy, with no significant decoding differences in the left  
201 occipital, left parietal, or left temporal lobes (**Supplementary Figure 2B**).

202 Visualization of the anatomical structure of informational connectivity (**Figure 4C**) con-  
203 firmed increased connectivity in the attended condition compared to the unattended condition  
204 in the early-1 and late time windows. In contrast, T2 network connectivity was stronger in the  
205 unattended condition in the early-2 time window, consistent with the delayed closeness central-  
206 ity peak shown in **Figure 4B** and **Figure 4D**. After FDR correction for multiple comparisons,  
207 the early-1 window showed significant connectivity differences between the occipital and tem-  
208 poral lobes as well as between the parietal and temporal lobes ( $p < 0.05$ ).

209 In summary, both T1 and T2 showed attentional enhancements of informational connectivity  
210 between the occipital and temporal lobes, which occurred at intermediate and late time windows  
211 after T1 but at an early time window after T2. Meanwhile, T2 showed a striking delay in  
212 informational connectivity enhancement when T1 was attended, which did not occur for T1.

213 **Informational network dynamics during the transition from T1 to T2 pro-**  
 214 **cessing**



**Figure 5.** Axial view of the difference in informational connectivity between attended and unattended conditions during the transition from T1 to T2 processing. The first column shows the difference in T1 informational connectivity at the intermediate window (same data as in **Figure 3C**), occurring just before T2. The second and third columns show the difference in T2 informational connectivity at the early-1 and early-2 windows (same data as in **Figure 4C**), occurring just after T2. The presented edges in the first row are significant at  $p < 0.01$  compared to a shuffled null distribution. Edges with higher values are shown in red, indicating greater connectivity during the attended than the unattended condition. The second row presents the FDR corrected edges ( $p < 0.05$ ). The inset T1-T2 transition timeline shows the T1 processing timeline and T2 processing timeline over the same time axis.

215 We next examined the anatomical organization of attention-modulated networks during the  
 216 transition from T1 to T2 processing. When T1 was attended, the enhancement of T1 attended  
 217 informational connectivity in the intermediate time window, right before T2, was left later-  
 218 alized (**Figure 5, first column**). There were individual edges strongly connected ( $p < 0.01$   
 219 uncorrected) the left rostral middle frontal, pars opercularis and posterior cingulate (see **Sup-**  
 220 **plementary Figure 3**) regions in the frontal and cingulate lobes, which also showed enhanced  
 221 decoding performance in the same time window (Zhu et al., 2024). After FDR correction for  
 222 multiple comparisons, there were also significant connectivity differences between the left oc-  
 223 cipital and frontal lobes and between frontal and cingulate lobes ( $p < 0.05$ ) in the T1 interme-

224 diate window.

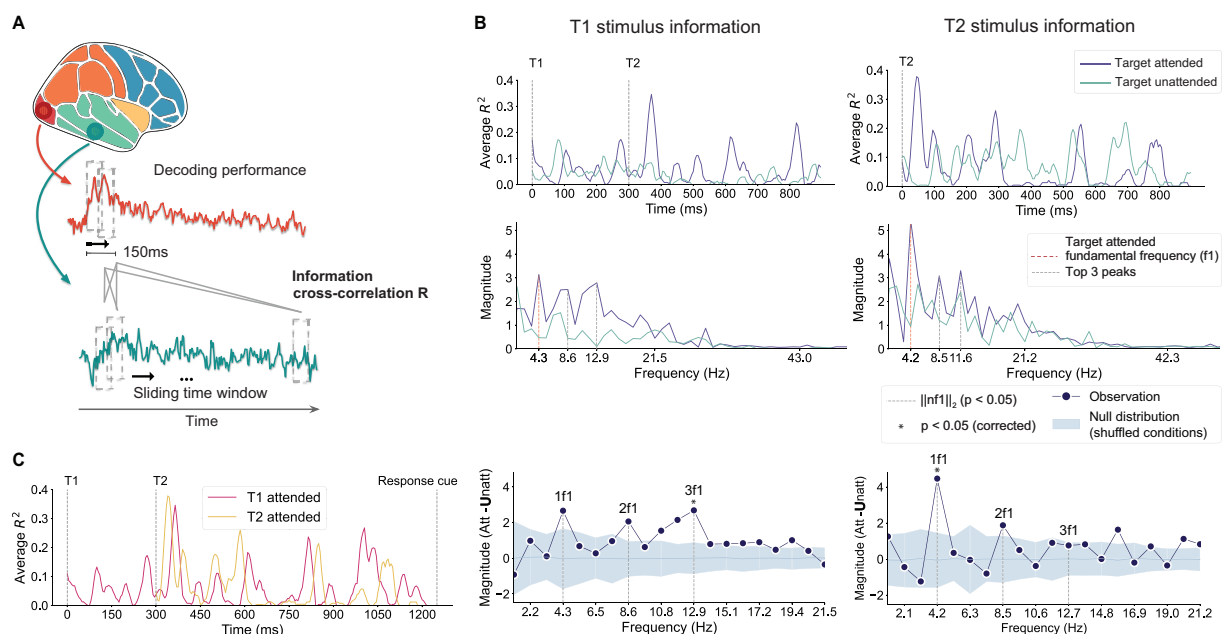
225 When T2 was attended, attentional enhancements in the early-1 window, just after T2 onset,  
226 were similarly left lateralized (**Figure 5, second column**). After FDR correction for multi-  
227 ple comparisons, there were also significant connectivity differences between the temporal and  
228 frontal lobes ( $p < 0.05$ ) in the T2 early-1 window. However, when T1 was attended and T2  
229 was unattended, T2 informational connectivity was delayed (early-2 window) and right later-  
230 alized (**Figure 5, third column**). After FDR correction for multiple comparisons, there were  
231 significant connectivity differences between the parietal and temporal lobes ( $p < 0.05$ ) in the  
232 T2 early-2 window.

233 Thus, just before and after the onset of T2, attention to T1 and to T2, respectively, increased  
234 informational connectivity along a left-lateralized pathway involving the occipital and frontal  
235 lobes.

### 236 **An early occipital motif recurred in the entorhinal-parahippocampal cor-** 237 **tex**

238 From the connectivity results above, we found that temporal attention enhanced informational  
239 connectivity between the occipital and temporal lobes for both targets. Temporal lobe regions  
240 subserving memory can be modulated by spatial attention (Wilming et al., 2018; Aly and Turk-  
241 Browne, 2016), and visual short-term memory plays a role in the current temporal attention  
242 task due to the requirement to wait for the response cue presented 1 s after T2 to know which  
243 stimulus to report. Therefore, we next asked how information was dynamically shared between  
244 the occipital lobe and the atlas-based regions within the temporal lobe most closely associated  
245 with memory, namely the entorhinal and parahippocampal cortex.

246 We asked how early visual information captured in the initial sensory response might be  
247 replayed in the entorhinal-parahippocampal cortex across time. To do so, we measured the



**Figure 6.** Temporal attention rhythmically modulated sharing of stimulus information between occipital and entorhinal-parahippocampal cortex. **(A)** Schematic of dynamic information cross-correlation R analysis. Stimulus information decoded from occipital cortex (0-150 ms after target onset) are cross correlated with decoded representations in the entorhinal-parahippocampal cortex using sliding windows (5 ms stride and 50 ms window size). **(B)** The  $R^2$  time series (top row) averaged across the 150 ms after target onset for T1 (left) and T2 (right) stimulus information. FFT of the  $R^2$  time series by attention condition (middle row) and their difference (bottom row). The attended  $R^2$  time series exhibited periodicity around a fundamental frequency of 4 Hz for both T1 and T2. **(C)** The  $R^2$  time series for both T1 attended and T2 attended conditions overlaid on the same time axis. It shows that in a hypothetical scenario in which both targets would be attended and there would be no processing trade-offs, the peaks of the  $R^2$  between the occipital and entorhinal-parahippocampal cortices for T1 and T2 roughly coincide.

248 relation between orientation information in the occipital lobe within the first 150 ms after tar-  
249 get onset and information in the entorhinal–parahippocampal cortex across time by calculating  
250 the correlation between their decoding time series using sliding time windows (**Figure 6A**).  
251 For both T1 and T2, the correlation time series for the attended condition seemed to exhibit a  
252 periodic pattern (**Figure 6B, first row**).

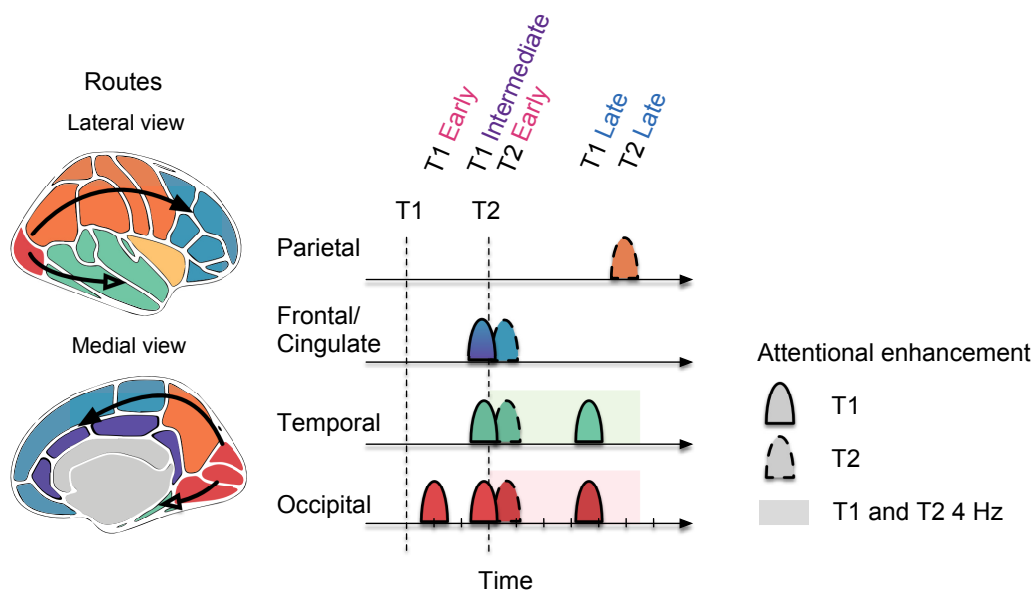
253 This observation was confirmed by applying FFTs to the correlation time series and com-  
254 paring the resulting frequency spectra for attended and unattended conditions. For both targets,  
255 the spectra for the attended condition peaked at multiples of 4 Hz, indicating a periodic fluc-  
256 tuation with a 4 Hz fundamental frequency (**Figure 6B, second row**). The total energy of the  
257 harmonics (see **Methods, Frequency analysis**)—the combined power of the first harmonic (4  
258 Hz) plus the second and third harmonics (8 and 12 Hz)—was significantly greater for attended  
259 than for unattended conditions for each target, as established by permutation tests compared to  
260 the null distribution ( $p < 0.05$ ).

261 Overlaying the correlation time series for the T1 attended and T2 attended conditions (**Fig-**  
262 **ure 6C**) shows that the periodic pattern peaks at similar times after T2 onset. This overlap may  
263 suggest that, if a participant were attending both targets in a hypothetical scenario with no pro-  
264 cessing trade-offs, there would be competition between their representations in memory-related  
265 regions.

## 266 **Discussion**

267 We found that temporal attention to one of two targets (T1 and T2) presented in rapid succession  
268 dynamically modulated informational connectivity across cortical networks. These attention-  
269 related shifts in connectivity occurred during both early and late time windows and were largely  
270 independent of corresponding attentional changes in decoding accuracy. This dissociation in-  
271 dicates that independent of amplifying stimulus representations, temporal attention alters how

272 stimulus information is routed across networks. These findings suggest that temporal attention  
273 leads to selective routing, which may serve to resolve competition between stimuli for com-  
274 munication routes. Rather than simply increasing representational strength within a region,  
275 temporal attention biases how stimulus information is shared across network pathways at spe-  
276 cific moments in time. The attentional modulation of information routing was associated with  
277 the processing transition from T1 to T2 and with the theta-rhythmic recurrence of early occipital  
278 motifs in memory-related regions.



**Figure 7.** Conceptual illustration of dynamic selective routing. The two proposed pathways are indicated with arrows. In this scheme, competition occurs when T1 and T2 are processed consecutively, and temporal attention modulates the routing of stimulus information from occipital cortex (red) to two downstream areas before decision-making: frontal–cingulate cortex (blue and purple) and temporal cortex (green). The horizontal time axis shows periods when temporal attention enhances informational connectivity (ticks every 100 ms). The midpoint of each marked period of attentional enhancement is aligned with the midpoint of each significant time window. The enhancement periods shown include both significant time windows in which closeness centrality along a route was higher in attended than unattended conditions, as well as windows in which informational connectivity along a route was stronger when a stimulus was attended than when it was unattended (informational connectivity network edges,  $p < 0.05$  corrected). For all lobes, T1 and T2 attentional modulations are plotted on the same time axis. The shaded strip along the time axis for occipital and temporal cortex represents the 4 Hz periodic occipital motif in the entorhinal–parahippocampal cortex found for both T1 and T2. Attentional enhancements were left lateralized in all lobes except parietal.

279 **Early and late attentional modulations of informational connectivity for**  
280 **each target**

281 Attention modulated informational connectivity network structure mainly at both early and late  
282 windows for each target (summarized in [Figure 7](#)), measured by spatial patterns of closeness  
283 centrality. Early modulations occurred  $\sim 100$  ms after each target, around the time when early  
284 visual event-related responses (Doherty et al., 2005; Correa et al., 2006) and orientation de-  
285 coding (Cichy et al., 2015; Wardle et al., 2016; Pantazis et al., 2018) ramp up. Unlike spatial  
286 attention (van Es et al., 2018; Dugué et al., 2020; Liu et al., 2021) and feature-based attention  
287 (Maunsell and Treue, 2006; Liu et al., 2007; Foster and Ling, 2022), which modulate early  
288 visual representations, studies of temporal attention have failed to find early increases in uni-  
289 variate responses or multivariate representations after target onset when temporal expectation  
290 is controlled (Zhu et al., 2024). Our results indicate that temporal attention may instead exert  
291 early effects without altering local encoding strength by selective routing from visual regions.

292 In the early window, T1 showed attentional enhancements of closeness centrality primarily  
293 in the occipital lobe (T1 early in [Figure 7](#)), whereas T2 showed attentional enhancements of  
294 closeness centrality in both occipital and temporal lobes (T2 early in [Figure 7](#)). Thus, even at  
295 early latencies traditionally associated with feedforward processing, temporal attention modi-  
296 fies communication structure rather than local gain. Late modulations diverged between targets.  
297 In the late time window, T1 showed increased closeness centrality in the occipital and temporal  
298 lobes (T1 late in [Figure 7](#)), but no such effect was significant for T2. Instead, the late window  
299 for T2 exhibited a mixture of enhanced closeness centrality in the parietal lobe (T2 late in [Fig-](#)  
300 [ure 7](#)) and weak increases in informational connectivity between specific occipital and temporal  
301 lobe regions ([Supplementary Figure 4](#)) that did not survive multiple comparisons correction.  
302 One possible account of this variability in late connectivity patterns for T2 is that participants  
303 can engage different routing strategies to maintain T2 information until the response window:

304 sharing information with either the temporal lobe (similar to T1) or the parietal lobe. The in-  
305 volvement of the posterior parietal cortex in late T2 routing aligns with its established role  
306 in maintaining task-relevant information when visual stimuli are no longer present, in spatial  
307 attention-driven and visual working memory tasks (Todd and Marois, 2004; Xu, 2018a; Dugué  
308 et al., 2018; Xu, 2024). It has been argued that such maintenance does not only depend on pos-  
309 terior parietal cortex, but selectively uses visual information relayed from occipital-temporal  
310 cortex according to task demands (Xu, 2018b). The overall weaker late attentional modulation  
311 for T2 may also reflect lower competitive demands during this window, as much of T1 process-  
312 ing may be complete by this time ( $\sim 800$  ms after T1). Importantly, this pattern indicates that  
313 routing is flexible—attention dynamically allocates information to distinct maintenance systems  
314 depending on task timing and competition.

### 315 **Pathways for selective routing**

316 The distinct temporal windows of modulation may correspond to distinct pathways that are  
317 competitively accessed by both targets. The current findings point to two pathways for selective  
318 routing—one during the transition from T1 to T2 involving the fronto-cingulate cortex, and the  
319 other after both targets appear involving the temporal lobe (the two pathways are visualized in  
320 [Figure 7](#)).

321 ***Fronto-cingulate routing during the T1-T2 transition.*** First, during the transition from T1  
322 to T2, attentional modulations of informational connectivity suggest selective routing to the left  
323 fronto-cingulate cortex. In a previous study using the same dataset, we found that temporal at-  
324 tention increased T1 decoding in left fronto-cingulate cortex immediately before T2 onset (Zhu  
325 et al., 2024). Here we demonstrate that this time window is also characterized by attention-  
326 enhanced informational connectivity associated with T1 (T1 intermediate in [Figure 7](#)) along

327 left-lateralized pathways involving the fronto-cingulate cortex. Immediately after T2 onset, at-  
328 tended T2 also engaged a left-lateralized pathway extending into the left frontal cortex (T2 early  
329 in [Figure 7](#)), whereas unattended T2 showed delayed and right-lateralized routing. Uncorrected  
330 connectivity networks showed that this right-lateralized pathway ultimately crossed over to the  
331 left frontal cortex.

332 We speculate that a possible explanation for these results is that sequential targets compete  
333 for access to a left fronto-cingulate bottleneck during the T1 to T2 transition, and temporal  
334 attention modulates this routing process. The cingulo-opercular (CO) network has been im-  
335 plicated in selecting a retrocued item and reformatting it into an action-oriented representation  
336 during visual working memory tasks (Wallis et al., 2015; Myers et al., 2017). Given that target  
337 orientations must be maintained until the response cue in the present task, such a selection and  
338 reformatting operation would be relevant here. Thus, temporal attention may resolve competi-  
339 tion between T1 and T2 through biased access to large-scale communication pathways.

340 ***Medial-temporal routing and theta-rhythmic replay.*** Second, we found evidence for attention-  
341 mediated selective routing to memory-related regions in the temporal lobe. Entorhinal cortex  
342 and parahippocampal cortex are key regions interconnected with hippocampus within the me-  
343 dial temporal lobe to support memory (Lavenex and Amaral, 2000; Ranganath and Ritchey,  
344 2012; Knierim et al., 2014). Early occipital decoding dynamics appeared to be replayed in these  
345 regions rhythmically at 4 Hz throughout the trial. This fundamental frequency falls within the  
346 theta band—a frequency range associated with memory-related activity in the medial temporal  
347 lobe (Herweg et al., 2020; Lega et al., 2012). Critically, this replay occurred only when stimuli  
348 were attended. Both targets showed this periodic replay pattern when attended, with similar  
349 absolute timing during the trial (the timing of the periodic replay coincides with T2 early and  
350 both T1 and T2 late in [Figure 7](#)).

351 These findings suggest that only one target representation can be actively maintained through  
352 periodic replay in the medial temporal lobe, and that attention regulates which one is main-  
353 tained. Thus the medial temporal lobe may be a site of competition for representational re-  
354 sources following the appearance of both targets, leading to selective routing. Together with the  
355 frontal–cingulate findings, this observation suggests the presence of at least two bottlenecks in  
356 the network: one governing selection during target transition and another governing oscillatory  
357 maintenance after stimulus encoding.

### 358 **Network communication mechanisms for temporal attentional selection**

359 The early and late attentional modulations observed in the informational connectivity network  
360 following target onset suggest that stimulus information is communicated neither instanta-  
361 neously in a single phase nor continuously over time. Instead, spatial patterns of closeness  
362 centrality differed between attended and unattended networks across multiple discrete time win-  
363 dows: for T1 these included early (50–175 ms), intermediate (250–385 ms), and late (625–780  
364 ms) periods; for T2, differences emerged during early (25–215 ms) and late (450–580 ms) win-  
365 dows. This temporal segmentation suggests that stimulus information is transmitted at discrete  
366 intervals, each providing a distinct window for network-wide exchange.

367 One mechanistic interpretation is that stimulus information is conveyed as a “packet,” a term  
368 from computer science that refers to a small, formatted unit of data designed to travel efficiently  
369 over network connections. Analogous to computer network communication—where a packet  
370 can be sent at different times or routed through different paths (Cerf and Kahn, 1974; McQuil-  
371 lan et al., 1980; Gallager, 2003)—a packet of neural information may likewise be transmitted  
372 at distinct moments via neural routes. Computer science also provides an interesting, albeit  
373 speculative, analogy for selective routing. In the “store-and-forward” mechanism in computer  
374 networks (McQuillan and Walden, 1977; Heart et al., 1970), each node buffers and forwards

375 data packets in sequence. Thus information must be buffered in limited-capacity nodes before  
376 being relayed downstream.

377 The present results suggest fronto-cingulate cortex and entorhinal-parahippocampal cortex  
378 as two candidate regions that may function as limited-capacity buffers that maintain and forward  
379 prioritized stimulus information in the current task. Temporally segmented routing may explain  
380 why attentional modulations of informational connectivity appear at multiple, distinct moments  
381 rather than as a continuous flow.

382 Altogether, investigating informational connectivity dynamics and their attentional modula-  
383 tion reveals stimulus processing as a network-level phenomenon. Such a perspective advances  
384 understanding of how the brain routes information across large-scale cortical networks during  
385 fast-paced, dynamic tasks.

## 386 **Conclusion**

387 Here, we provide evidence that temporal attention modulates how, when, and through which  
388 pathways stimulus-information travels, rather than simply how strongly it is represented. Be-  
389 yond enhancing neural responses, temporal attention thus engages a selective routing mech-  
390 anism to prioritize stimulus information at a specific moment in time. When participants at-  
391 tended to one of two rapidly presented sequential targets, temporal attention modulated infor-  
392 mational connectivity across two main pathways: an occipito–frontal–cingulate route involved  
393 in selection during the transition between targets, and an occipito–temporal route supporting  
394 theta-rhythmic maintenance in the medial temporal lobe. The two sequential targets appeared  
395 to compete for access to these routes. Temporal attention modulated informational access to  
396 these routes through two complementary mechanisms: discrete bursts of network communica-  
397 tion occurring throughout the trial, with a concentration during the transition from the first to the  
398 second target, and theta-rhythmic activity that persisted for an extended period following both

399 targets. By identifying routing as the mechanism through which temporal attention resolves  
400 sequential competition, this research reveals a network-level account of temporal attention and  
401 offers a new framework for understanding how the brain manages information flow during fast,  
402 dynamic cognition.

## 403 **Methods**

### 404 **Observers**

405 Ten observers (5 females, mean age = 29 years old, SD = 4 years), including authors RND and  
406 KJT, participated in the study. Each observer first completed one behavioral training session,  
407 followed by two separate 2-hour MEG recording sessions conducted on different days, yielding  
408 a total of 20 MEG sessions. Collecting two sessions per observer enabled us to assess within-  
409 observer reliability across sessions and follows an approach used in other MEG studies of vision  
410 to collect multiple sessions per observer (Kok et al., 2017; Besserve et al., 2007). Experimental  
411 protocols were approved by the University Committee on Activities involving Human Subjects  
412 at New York University. All observers had normal or corrected-to-normal vision using MR safe  
413 lenses. All observers provided informed consent.

### 414 **Stimuli**

415 Stimulus presentation was programmed in MATLAB using Psychtoolbox (Brainard and Vision,  
416 1997; Pelli and Vision, 1997; Kleiner et al., 2007) and run on an iMac. During MEG acquisition,  
417 images were delivered with an InFocus LP850 projector (Texas Instruments, Warren, NJ) and  
418 reflected by a mirror onto a translucent screen (1024 × 768 pixels; 60 Hz) positioned 42 cm from  
419 the participant. Stimuli appeared on a mid-gray background (206 cd/m<sup>2</sup>), and timing accuracy  
420 was verified with a photodiode. For the behavioral training conducted outside the MEG, stimuli  
421 were shown on a gamma-corrected Sony Trinitron G520 CRT monitor (1024 × 768 pixels; 60

422 Hz) at a viewing distance of 56 cm. Participants maintained a stable head position using a  
423 combined chin-and-head rest.

424 **Visual targets.** Targets were foveally presented, full-contrast sinusoidal gratings (1.5 cy-  
425 cles/deg). Each grating subtended  $4^\circ$  in diameter and was windowed with a raised-cosine  
426 smooth taper so that the outermost  $0.4^\circ$  gradually fell to zero contrast.

427 **Auditory cues.** Both precues and response cues were 100-ms pure-tone sinusoids, gated  
428 with 10-ms cosine ramps at onset and offset to minimize audible transients. A high tone (1046.5  
429 Hz; C6) signaled T1, whereas a low tone (440 Hz; A4) signaled T2.

## 430 **Task**

431 Observers were instructed to voluntarily direct their temporal attention to a specific time point  
432 and report the tilt of the cued target. On each trial (ref to [Figure 1A](#)), two visual targets (T1  
433 and T2) were presented sequentially at the same spatial location. Each target appeared for 50  
434 ms, with a 300 ms stimulus onset asynchrony (SOA) between them—a timescale known to  
435 elicit temporal attentional tradeoffs in prior psychophysical work (Denison et al., 2017, 2021;  
436 Fernández et al., 2019; Palmieri and Carrasco, 2024). Each target was slightly tilted either  
437 clockwise (CW) or counterclockwise (CCW) relative to either the vertical or horizontal axis  
438 ([Figure 1B](#)); tilt direction and axis were manipulated independently and counterbalanced for  
439 each target.

440 Each trial began with an auditory precue occurring 1,050 ms prior to target presentation that  
441 instructed observers to allocate attention to T1 or T2 (high vs. low tone). A second auditory  
442 cue, presented 950 ms after the targets, specified which target should be reported. Participants  
443 indicated the tilt direction (CW vs. CCW) using a two-button response within 1,500 ms. Feed-  
444 back was conveyed at the end of the trial by changing the color of the fixation marker (green for  
445 correct, red for incorrect, blue for timeout).

446 On each trial, the timing of target presentation was fully predictable following the auditory  
447 precue. The attended target varied from trial to trial based on the precue, while the target  
448 designated for behavioral report was determined by a separate response cue presented at the  
449 end of each trial. In 80% of trials, the precue directed attention to a single target (T1 or T2),  
450 and in those cases, the response cue matched the precued target 75% of the time—creating an  
451 incentive for participants to follow the precue. Both the identity of the precued target and the  
452 cue validity (match vs. mismatch of precue and response cue) were randomized across trials.  
453 Each MEG session included 192 trials each for precue T1 and precue T2 conditions. Trials  
454 were labeled as “attended” with respect to the precued target and “unattended” with respect to  
455 the non-target on that trial, resulting in 192 attended and 192 unattended trials per target. Note  
456 that the response cue allowed us to verify that behavior depended on cue validity; however,  
457 because the response cue was presented after both targets at the end of the trial, it was irrelevant  
458 to the conditions used for decoding. Additionally, the identity of the auditory precue (high vs.  
459 low tone) was orthogonal to the stimulus orientation (vertical or horizontal) and thus carried no  
460 information relevant to decoding the visual representation.

461 The experiment also included neutral trials (20% of all trials), which were cued with a  
462 combination of the high and low tones, providing no temporal information and thus indicat-  
463 ing that attention should be distributed across both targets. These trials enabled behavioral  
464 assessment of temporal attentional selectivity (see [Supplementary Figure 1](#)). Due to their  
465 reduced count—50% fewer trials relative to the precue-T1 and precue-T2 conditions—neutral  
466 trials were excluded from MEG decoding analyses to avoid trial-count imbalances that could  
467 bias classification performance.

468 **Training.** Prior to MEG recording, participants completed a behavioral training session to  
469 familiarize them with the task and calibrate individual tilt discrimination thresholds. Tilt magni-  
470 tude was adjusted separately for each observer using a 3-up-1-down staircase procedure to target

471 approximately 79% accuracy on neutral trials (mean threshold tilt =  $0.76^\circ$  across observers).

## 472 **Eye tracking**

473 Throughout each trial, observers fixated on a central circular marker ( $0.15^\circ$  diameter). Eye po-  
474 sition was continuously recorded at 1000 Hz using an EyeLink 1000 system (SR Research).  
475 Calibration was performed at the beginning of each session using a five-point grid, which al-  
476 lowed gaze coordinates to be mapped to degrees of visual angle.

## 477 **MEG acquisition**

478 Each MEG session consisted of 12 experimental blocks, each lasting approximately 6 minutes.  
479 Observers were allowed to rest between blocks and resumed the task at their own pace by  
480 pressing a button to continue.

481 Prior to MEG acquisition, individual head shapes were digitized using a FastSCAN laser  
482 scanner (Polhemus, VT, USA). Fiducial points were marked digitally at the nasion, forehead,  
483 and bilaterally at the tragus and peri-auricular locations. The positions of these reference points  
484 were recorded at both the beginning and end of each session. To enable co-registration of head  
485 position with MEG sensor locations, electrodes were affixed at the forehead and peri-auricular  
486 sites corresponding to the digitized fiducials.

487 MEG signals were acquired continuously using a 157-channel axial gradiometer system  
488 (Kanazawa Institute of Technology, Kanazawa, Japan) housed in the KIT/NYU MEG facility  
489 at New York University. Background magnetic interference was tracked using three orthogo-  
490 nal reference magnetometers placed approximately 20 cm from the sensor array. Data were  
491 sampled at 1000 Hz, with online DC correction and a high-pass filter set at 200 Hz.

## 492 **Preprocessing**

493 MEG preprocessing was conducted in MATLAB using the FieldTrip toolbox for EEG/MEG  
494 analysis (Oostenveld et al., 2011), following these steps: 1) All trials were visually examined,  
495 and those containing eye blinks or other artifacts were manually excluded. Across sessions,  
496 the number of rejected trials ranged from 18 to 88 (3.49–17.05%), with a mean of 51.75 trials  
497 (10.03%) and a standard deviation of 20.06. 2) Channels exhibiting abnormally high or low  
498 variability were automatically flagged based on their time series standard deviations. 3) Time  
499 series from these noisy channels were replaced by spatial interpolation from neighboring sen-  
500 sors. The number of interpolated channels per session ranged from 0 to 6 (0–3.82%), with a  
501 mean of 3.85 (2.45%) and a standard deviation of 1.50. 4) To remove environmental noise,  
502 signals from the reference magnetometers were linearly regressed out of the MEG sensor time  
503 series.

## 504 **Source reconstruction**

505 We performed source reconstruction using MNE Python (Gramfort et al., 2013). For each  
506 participant, we generated a cortical surface mesh from their anatomical MRI with 4,000 ver-  
507 tices per hemisphere. Coregistration between MEG and MRI data was performed automatically  
508 using three fiducial landmarks (nasion and bilateral peri-auricular points) and digitized scalp  
509 points acquired via laser scanning (Gramfort et al., 2013; Houck and Claus, 2020). Forward  
510 models were calculated using a single-shell Boundary Element Model (BEM) to approximate  
511 the head's geometry and tissue conductivities. Source estimates were computed by inverting  
512 the forward model using dynamic statistical parametric mapping (dSPM) (Dale et al., 2000). At  
513 each vertex, the estimated source activity was modeled as a dipole oriented perpendicular to the  
514 cortical surface. The sign of the dipole reflects current direction—positive for outward, nega-  
515 tive for inward flow (Wang et al., 2023). In dSPM-based source localization, the typical Dipole

516 Localization Error (DLE) is approximately 2 cm, and the Spatial Dispersion (SD) is around 4  
517 cm (Hauk et al., 2011; Hedrich et al., 2017). DLE represents the Euclidean distance between  
518 the true dipole location and the maximum of the estimated source map, while SD captures the  
519 extent to which the estimated activity is spatially spread around the true source location (Molins  
520 et al., 2008; Hauk et al., 2011).

521 Cortical parcellation was performed using the 34 regions per hemisphere defined in the  
522 Desikan–Killiany (DK) atlas (Desikan et al., 2006). These regions of interest (ROIs) can be  
523 grouped into broader anatomical lobes (occipital, parietal, temporal, frontal, cingulate and in-  
524 sula) following the mapping scheme in (Klein and Tourville, 2012).

## 525 **Decoding**

526 To decode stimulus orientation (vertical vs. horizontal), we trained linear support vector ma-  
527 chine (SVM) classifiers independently at each time point (Cichy et al., 2015; King and Dehaene,  
528 2014). A 5-fold cross-validation was used to partition trials into training and testing sets, en-  
529 suring unbiased estimates of classification performance. Decoding was performed separately  
530 for each target (T1 and T2) under each precue condition, resulting in time-resolved decoding  
531 accuracy time series. For instance, in decoding T1 orientation, trials with a precue to T1 were  
532 labeled as attended, while those cued to T2 were considered unattended. To improve signal-to-  
533 noise ratio, we generated pseudotrials by averaging across small groups of 5 trials (Isik et al.,  
534 2014; Meyers, 2013; Wardle et al., 2016), and also averaged the data over 5 ms temporal win-  
535 dows (Isik et al., 2014). The entire decoding process was repeated 100 times using randomized  
536 pseudotrial assignments to mitigate any variability introduced by the averaging procedure.

537 In source space, we performed decoding of stimulus orientation using estimated source  
538 activations within anatomically defined ROIs from the DK atlas (see *Source reconstruction*).  
539 Each ROI contained multiple vertices, and the corresponding time series were derived from

540 the source reconstruction output. Because the number of features (vertices) within an ROI  
541 often exceeded the number of available samples (trials), we applied dimensionality reduction  
542 to prevent overfitting. Specifically, for ROIs containing more than 100 vertices, we employed  
543 univariate feature selection using an ANOVA F-test (Pedregosa et al., 2011; Gramfort et al.,  
544 2013), applied only to the training set within the 5-fold cross-validation. The top 100 vertices  
545 with the highest F-scores were selected as input features for the classifier, ensuring that the  
546 feature dimensionality did not exceed 100 for any ROI.

547 To obtain decoding performance for larger regions (e.g., occipital and entorhinal–parahippocampal  
548 cortex), we averaged decoding accuracy across the constituent ROIs within each region.

## 549 **Dynamic informational connectivity analysis**

### 550 **Network construction**

551 To obtain higher signal-to-noise stimulus information, we averaged decoding accuracy time  
552 series from source-reconstructed atlas-based regions ( $N = 68$  regions, or 34 per hemisphere)  
553 across all sessions per attention condition to form a “super-subject” and conducted all further  
554 analyses using these data. We estimated informational connectivity networks based on the  
555 decoding accuracy timeseries of the “super-subject”. We performed this analysis across sliding  
556 time windows to understand how informational connectivity changes across time, a dynamic  
557 informational connectivity analysis. Formally, each region  $i \in V = \{1, \dots, N\}$  was treated  
558 as a node in a graph. For each time  $t$ , we estimated a weighted undirected graph  $G(t) =$   
559  $(V, E, \mathbf{Z}(t))$ , where  $E = (i, j)$  is the set of all possible undirected edges between region  $i$   
560 and another region  $j \in V$ ,  $\mathbf{Z}(t) = [Z_{ij}(t)]$  is the adjacency matrix encoding informational  
561 connectivity.

562 For each time  $t$ , we define a sliding window of width  $\Delta t$ , denoted  $W(t) = [t, t + \Delta t]$ , where  
563  $\Delta t$  contains discrete time steps  $\tau_l \in \{\tau_1, \dots, \tau_m\}$ . Here, each time step  $\tau_l$  was defined as a 5

564 ms bin (see details in *Decoding*) and the window duration was 50 ms (i.e.,  $m = 10$ ). Within  
565 each window  $W(t)$ , the stimulus orientation decoding accuracies for each region  $i$  are denoted  
566 by  $\mathbf{a}_i(t) = (a_i(t + \tau_1), a_i(t + \tau_2), \dots, a_i(t + \tau_m)) \in \mathbb{R}^m$ .

567 Informational connectivity between regions  $i$  and  $j$  at time  $t$  is defined as the Pearson cor-  
568 relation between their accuracy vectors using [Equation 1](#):

$$Z_{ij}(t) = \text{corr}(\mathbf{a}_i(t), \mathbf{a}_j(t)). \quad (1)$$

569 Thus, by sliding the window across time, we generate a time-varying network  $\{G(t)\}$ , which  
570 captures the evolution of informational connectivity across conditions.

### 571 Closeness Centrality

572 Closeness centrality is a graph-theoretic measure that summarizes the distance between one node  
573 in the network and all other nodes and quantifies how efficiently signals can spread through  
574 a network (Freeman et al., 1979). Here we used correlation distances to calculate closeness  
575 centrality for each atlas-based region, providing a summary of each region's shared information  
576 with all other regions in each sliding time window, and thus the centrality of that region within  
577 the informational connectivity network across time.

578 For each region  $i \in V$ , we define its closeness centrality with respect to the informational  
579 connectivity network  $G(t)$  in [Equation 2](#):

$$C_i(t) = \frac{N - 1}{\sum_{j \neq i} d_{ij}(t)}, \quad (2)$$

580 where  $d_{ij}(t)$  denotes the shortest correlation distance between regions  $i$  and  $j$ , given by  
581 [Equation 3](#):

$$d_{ij}(t) = 1 - Z_{ij}(t). \quad (3)$$

582 Thus,  $C_i(t)$  represents the average inverse correlation distance from region  $i$  to all other  
583 regions, with larger values indicating stronger and more efficient information flow.

584 For a given lobe, the closeness centrality was calculated as the L2-norm of the centrality  
585 values for each ROIs within the lobe, providing a measure of overall centrality strength.

## 586 **KL Divergence**

587 Kullback-Leibler (KL) divergence is an information-theoretic measure that summarizes how  
588 different one probability distribution is from another. In statistics and machine learning, it  
589 is used to quantify the information loss incurred when an approximate distribution is used in  
590 place of a reference distribution (Kullback and Leibler, 1951; Cover, 1999). Here, we use  
591 the distribution of closeness centrality to summarize global network structure. We then use  
592 KL divergence to compare network structure across attention conditions within each sliding  
593 time window, providing a summary of how strongly the attended and unattended informational  
594 connectivity networks diverge over time.

595 Let  $\mathcal{C}^{(c)}(t) = \{C_i^{(c)}(t)\}_{i=1}^N$  denote the set of region-wise closeness centrality values at time  
596  $t$  under condition  $c$ . We normalize these values to obtain a distribution of scaled closeness  
597 centrality values across regions using [Equation 4](#):

$$P_i^{(c)}(t) = \frac{C_i^{(c)}(t)}{\sum_{i=1}^N C_i^{(c)}(t)} \quad \text{for } i = 1, \dots, N. \quad (4)$$

598 To compare the attended ( $c = \text{att}$ ) and unattended ( $c = \text{unatt}$ ) networks, we compute the  
599 KL divergence, which is a relative entropy measure of the difference between two distributions  
600 using [Equation 5](#):

$$D_{\text{KL}}(P^{(\text{att})}(t) \parallel P^{(\text{unatt})}(t)) = \sum_{i=1}^N P_i^{(\text{att})}(t) \log \frac{P_i^{(\text{att})}(t)}{P_i^{(\text{unatt})}(t)}. \quad (5)$$

## 601 Information cross-correlation (time-lagged connectivity)

602 We used a cross-correlation approach to investigate whether an early motif in one region re-  
603 curred in other regions.

604 For region  $i$ , consider sliding windows  $W(t_i)$  with  $t_i \in \mathcal{T}_i = [0, 150]$  ms after target onset;  
605 for region  $j$ , windows  $W(t_j)$  with  $t_j \in \mathcal{T}_j$ . Let  $\mathbf{a}_i(W(t_i))$  and  $\mathbf{a}_j(W(t_j))$  denote the vectors of  
606 decoding accuracies extracted within those windows. Consistent with the sliding window used  
607 in previous sections, the window duration was 50 ms.

608 The cross-correlation between window  $W(t_i)$  and  $W(t_j)$  is using **Equation 6**:

$$R_{ij}(t_i, t_j) = \text{corr}\left(\mathbf{a}_i(W(t_i)), \mathbf{a}_j(W(t_j))\right). \quad (6)$$

609 We use Pearson correlation and it can expand explicitly as in **Equation 7**:

$$R_{ij}(t_i, t_j) = \frac{(\mathbf{a}_i - \bar{\mathbf{a}}_i)^\top (\mathbf{a}_j - \bar{\mathbf{a}}_j)}{\|\mathbf{a}_i - \bar{\mathbf{a}}_i\| \|\mathbf{a}_j - \bar{\mathbf{a}}_j\|}, \quad \mathbf{a}_i = \mathbf{a}_i(W(t_i)), \quad \mathbf{a}_j = \mathbf{a}_j(W(t_j)), \quad (7)$$

610 with  $\bar{\mathbf{a}}_i$  and  $\bar{\mathbf{a}}_j$  the within-window means. The collection  $\{R_{ij}(t_i, t_j)\}$  forms an  $|\mathcal{T}_i| \times |\mathcal{T}_j|$   
611 cross-correlation matrix for the pair  $(i, j)$ .

612 Here, for each sliding time window within the first 150 ms after target onset in the oc-  
613 cipital cortex (region  $i$ ), the cross-correlation with each sliding time window in the entorhi-  
614 nal–parahippocampal cortex (region  $j$ ) is denoted by  $R$  ( $R = R_{ij}(t_i, t_j)$ ). To summarize the  
615 early occipital pattern, we averaged  $R_{ij}(t_i, t_j)^2$  across  $t_i$  for each fixed  $t_j$ , thereby collapsing  
616 the  $|\mathcal{T}_i| \times |\mathcal{T}_j|$  matrix into a length- $|\mathcal{T}_j|$  time series of averaged  $R^2$  values for region  $j$ . Formally,  
617 we can use **Equation 8**:

$$\bar{R}_{ij}^2(t_j) = \frac{1}{|\mathcal{T}_i|} \sum_{t_i \in \mathcal{T}_i} R_{ij}(t_i, t_j)^2, \quad t_j \in \mathcal{T}_j. \quad (8)$$

## 618 **Frequency analysis**

619 For both T1 and T2, the averaged  $R^2$  values for the attended condition within the first 150 ms af-  
620 ter target onset in the occipital cortex has some periodic patterns in the entorhinal–parahippocampal  
621 cortex over time. We then applied FFT analysis for the  $R^2$  time series to quantify such period-  
622 icity.

623 We characterized periodic patterns in cross-correlation time series between regions of inter-  
624 est using a frequency analysis. Whereas a pure sinusoidal periodic waveform is characterized  
625 by a single frequency, a non-sinusoidal periodic waveform also has harmonics that reflect the  
626 strength of the periodic signal. The lowest frequency component of a periodic signal is the fun-  
627 damental frequency ( $f_0$ ), which determines the signal’s basic repetition rate. Harmonics refer  
628 to sinusoidal components of a signal that occur at integer multiples of a fundamental frequency  
629 ( $f_0$ ) as shown in **Equation 9**:

$$f_n = n \cdot f_0 \quad \text{for } n = 1, 2, 3, \dots \quad (9)$$

630  $f_1 = f_0$  (first harmonic),  $f_2 = 2f_0$  (second harmonic),  $f_3 = 3f_0$  (third harmonic), etc.

631 Here, we found a 4 Hz fundamental frequency, with 8 Hz and 12 Hz as its second and third  
632 harmonic frequencies, respectively, for both the T1 and T2 attended conditions. Specifically,  
633 we found 3 prominent peaks in the FFT and let the lowest frequency ( $f_1$ ) be the fundamental  
634 frequency. The other frequencies of the peaks are the multiplied frequencies for the lowest  
635 frequency (i.e.,  $2f_1, 3f_1$ ).

636 To quantify the overall strength of the periodic signal, we calculated harmonic energy as the  
637 L2-norm of harmonic amplitudes  $\|\mathbf{H}\|_2 = \sqrt{\sum_{n=1}^N H_n^2}$ , where  $H_n = |X(nf_1)|$  is the magnitude  
638 of the Fourier transform  $X(f)$  of the signal at the  $n$ -th harmonic frequency.

639 Here we simplified the notation by letting the amplitude of the  $n$ -th harmonic to be  $nf_1$ ,

640 and the harmonic energy to be  $\|nf1\|_2 = \sqrt{1f1^2 + 2f1^2 + 3f1^2}$  with  $n = 3$  (Appelbaum et al.,  
641 2010).

## 642 **Statistical analysis**

### 643 **General procedure**

644 **Null distribution construction.** To assess the statistical significance of the difference between  
645 attention conditions, we used nonparametric methods for the informational connectivity net-  
646 work. For a given measure (e.g., closeness centrality) we generated null distributions for the  
647 difference between attention conditions by randomly swapping or not swapping the condition  
648 labels (attended or unattended) session by session ( $n = 20$  sessions) for the decoding accuracy  
649 timeseries. We call these conditions with shuffled labels “pseudo-conditions.” To generate a  
650 null distribution for the effect of attention on a given measure of interest, we calculated the  
651 measure for each pseudo-condition in the same way as we had for the original conditions with  
652 correct labels, took the difference between “attended” and “unattended” pseudo-conditions, and  
653 repeated this randomization and analysis procedure 1000 times. For each target, the time win-  
654 dows of interest was 0–900 ms after the target onset, so the time range was not extended to the  
655 response cue and was comparable across targets

656 **Non-parametric cluster correction.** We used a non-parametric cluster correction for the  
657 time series of a given measure of interest, with measure-specific cluster correction methods  
658 described below. Significant time windows were identified as successive sliding windows in  
659 which informational connectivity measures survived cluster corrections. To do this, we first  
660 construct a null distribution of cluster statistics. The cluster-level statistic for each permutation  
661 was calculated as follows:

662 (1) For sample at each time step, get the difference of a given measure of interest (e.g.,  
663 closeness centrality) between two pseudo-conditions as the permuted value. The test statistic is

664 obtained by comparing the permuted value with the null distribution, previously generated for  
665 each time step as described in *Null distribution construction* or constructed more conservatively  
666 on empirical informational connectivity network. For more information on the null distribution  
667 model in network see Váša and Mišić (2022).

668 (2) Select all samples whose test statistic is larger than some threshold. Higher thresholds  
669 are better suited for identifying stronger, short-duration effects, whereas lower thresholds are  
670 better suited for identifying weaker, long-duration effects (Maris and Oostenveld, 2007). For  
671 example, threshold= 0.85 indicates that the permuted value is greater than the 85th percentile  
672 of the null distribution. Measure-specific thresholds are described in their respective sections  
673 below.

674 (3) Cluster the selected samples into connected sets on the basis of temporal adjacency.

675 (4) Calculate cluster-level statistics by taking the sum of the test statistic within a cluster.

676 (5) Take the largest of the cluster-level statistics.

677 **Reporting the significant windows.** In reporting significant time windows in the text, we  
678 give the starting time point of the first sliding window and the end time point of the last sliding  
679 window within the cluster. Visualizations shade the interval between the starting time points  
680 of the first and the last sliding windows to better match the plotted timeseries, where the value  
681 plotted at each time point represents the value derived from the 50 ms sliding window starting  
682 at that time point.

### 683 **Closeness centrality**

684 To assess the effect of temporal attention on closeness centrality across the full time series and  
685 identify time windows with significant differences between attention conditions, we used a non-  
686 parametric test with cluster correction as described in *Non-parametric cluster correction*. For  
687 the cluster-level statistic in each permutation, the null distribution generated for each time step

688 is described in the *Null distribution construction* The reported significant clusters are corrected  
689 with threshold values of 0.85, 0.95, or 0.99 (see figure captions).

### 690 **Informational connectivity network edges**

691 To assess the statistical significance of observed differences in informational connectivity net-  
692 work edges between attention conditions, we computed test statistics by comparing the observed  
693 values with the null distribution for each edge. Multiple comparisons across edges were then  
694 controlled using the Benjamini–Hochberg false discovery rate procedure. The edges for a spe-  
695 cific time window are constructed based on the averaged decoding accuracies across the time  
696 window.

### 697 **Cross-correlation frequency energy**

698 We sought to determine whether the cross-correlation time-series exhibited greater periodicity  
699 when a stimulus was attended vs. unattended. To do so, we assessed whether the harmonic  
700 energy of the major spectral peaks (4 Hz, 8 Hz, 12 Hz) differed between attention conditions,  
701 beyond what would be expected from a null distribution. We subtracted the unattended FFT  
702 spectrum from the attended ones and calculated the energy of the harmonics of this FFT spec-  
703 trum difference. We then compared the observed energy of the harmonics to a null distribution  
704 as described in *General procedure*.

### 705 **KL divergence**

706 We investigated how fluctuations in KL divergence from attended to unattended conditions  
707 across time deviated from the time-series of average KL divergence. To correct the test statistics  
708 for the full time series of the KL divergence, we used the same nonparametric cluster correction  
709 as described above *Non-parametric cluster correction*, using a conservatively constructed null  
710 distribution centered on the averaged KL value. The null distribution of networks is more con-

711 servative when constructing the null model from the empirical network (Váša and Mišić, 2022).  
712 Specifically, for each attention condition, we shuffled the empirical distribution of closeness  
713 centrality across time to construct a pseudo-condition. We then obtained the KL divergence be-  
714 tween the two pseudo-conditions. The null distribution of the KL divergence was generated by  
715 repeating this randomization and analysis procedure 1000 times. Therefore, for each time step,  
716 we have a histogram of 1000 KL values as a null distribution. Significant clusters reported are  
717 corrected with a fixed threshold of 0.6 for both T1 and T2. The significant cluster showed the  
718 time periods where the KL divergence is greater than the time-series of average KL divergence.

## 719 **Acknowledgments**

720 We thank Sirui Liu and Luis Ramirez for assistance with early versions of the experiment. We  
721 thank Hsin-Hung Li as well as members of the Denison and Carrasco Labs for helpful com-  
722 ments. We thank Jeffrey Walker at the NYU MEG lab for technical assistance. This research  
723 was supported by National Institutes of Health National Eye Institute R01 EY037358 and F32  
724 EY025533 to R.N.D., R01 EY019693 to M.C., T32 EY007136 to NYU, National Defense Sci-  
725 ence and Engineering Graduate Fellowship to K.J.T., and by funding from Boston University to  
726 R.N.D.

## 727 **References**

728 Aly, M. and Turk-Browne, N. B. (2016). Attention promotes episodic encoding by stabi-  
729 lizing hippocampal representations. *Proceedings of the National Academy of Sciences*,  
730 113(4):E420–E429.

731 Anton-Erxleben, K. and Carrasco, M. (2013). Attentional enhancement of spatial resolu-

- 732 tion: linking behavioural and neurophysiological evidence. *Nature Reviews Neuroscience*,  
733 14(3):188–200.
- 734 Anzellotti, S. and Coutanche, M. N. (2018). Beyond functional connectivity: investigating  
735 networks of multivariate representations. *Trends in Cognitive Sciences*, 22(3):258–269.
- 736 Appelbaum, L., Ales, J., Cottureau, B., and Norcia, A. (2010). Configural specificity of the  
737 lateral occipital cortex. *Neuropsychologia*, 48(11):3323–3328.
- 738 Banaie Boroujeni, K., Helfrich, R. F., Fiebelkorn, I. C., Bentley, J. N., Brunner, P., Lin, J. J.,  
739 Knight, R. T., and Kastner, S. (2025). High-frequency bursts facilitate fast communication  
740 for human spatial attention. *Nature Neuroscience*, pages 1–10.
- 741 Besserve, M., Jerbi, K., Laurent, F., Baillet, S., Martinerie, J., and Garnero, L. (2007). Classifi-  
742 cation methods for ongoing EEG and MEG signals. *Biological Research*, 40(4):415–437.
- 743 Bosman, C. A., Schoffelen, J.-M., Brunet, N., Oostenveld, R., Bastos, A. M., Womelsdorf, T.,  
744 Rubehn, B., Stieglitz, T., De Weerd, P., and Fries, P. (2012). Attentional stimulus selection  
745 through selective synchronization between monkey visual areas. *Neuron*, 75(5):875–888.
- 746 Brainard, D. H. and Vision, S. (1997). The psychophysics toolbox. *Spatial Vision*, 10(4):433–  
747 436.
- 748 Buschman, T. J. and Miller, E. K. (2007). Top-down versus bottom-up control of attention in  
749 the prefrontal and posterior parietal cortices. *Science*, 315(5820):1860–1862.
- 750 Carrasco, M. (2011). Visual attention: The past 25 years. *Vision Research*, 51(13):1484–1525.
- 751 Cerf, V. and Kahn, R. (1974). A protocol for packet network intercommunication. *IEEE Trans-*  
752 *actions on Communications*, 22(5):637–648.

- 753 Cichy, R. M., Ramirez, F. M., and Pantazis, D. (2015). Can visual information encoded in  
754 cortical columns be decoded from magnetoencephalography data in humans? *Neuroimage*,  
755 121:193–204.
- 756 Correa, Á., Lupiáñez, J., Madrid, E., and Tudela, P. (2006). Temporal attention enhances early  
757 visual processing: A review and new evidence from event-related potentials. *Brain research*,  
758 1076(1):116–128.
- 759 Coutanche, M. N. and Thompson-Schill, S. L. (2013). Informational connectivity: identifying  
760 synchronized discriminability of multi-voxel patterns across the brain. *Frontiers in Human*  
761 *Neuroscience*, 7:15.
- 762 Cover, T. M. (1999). *Elements of information theory*. John Wiley & Sons.
- 763 Dale, A. M., Liu, A. K., Fischl, B. R., Buckner, R. L., Belliveau, J. W., Lewine, J. D., and  
764 Halgren, E. (2000). Dynamic statistical parametric mapping: combining fMRI and MEG for  
765 high-resolution imaging of cortical activity. *Neuron*, 26(1):55–67.
- 766 Denison, R. N. (2024). Visual temporal attention from perception to computation. *Nature*  
767 *Reviews Psychology*, 3(4):261–274.
- 768 Denison, R. N., Carrasco, M., and Heeger, D. J. (2021). A dynamic normalization model of  
769 temporal attention. *Nature Human Behaviour*, 5(12):1674–1685.
- 770 Denison, R. N., Heeger, D. J., and Carrasco, M. (2017). Attention flexibly trades off across  
771 points in time. *Psychonomic Bulletin & Review*, 24:1142–1151.
- 772 Denison, R. N., Tian, K. J., Heeger, D. J., and Carrasco, M. (2024). Anticipatory and evoked vi-  
773 sual cortical dynamics of voluntary temporal attention. *Nature Communications*, 15(1):9061.

- 774 Desikan, R. S., Ségonne, F., Fischl, B., Quinn, B. T., Dickerson, B. C., Blacker, D., Buckner,  
775 R. L., Dale, A. M., Maguire, R. P., Hyman, B. T., et al. (2006). An automated labeling system  
776 for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest.  
777 *Neuroimage*, 31(3):968–980.
- 778 Doherty, J. R., Rao, A., Mesulam, M. M., and Nobre, A. C. (2005). Synergistic effect of  
779 combined temporal and spatial expectations on visual attention. *Journal of Neuroscience*,  
780 25(36):8259–8266.
- 781 Dugué, L., Merriam, E. P., Heeger, D. J., and Carrasco, M. (2018). Specific visual subregions  
782 of TPJ mediate reorienting of spatial attention. *Cerebral Cortex*, 28(7):2375–2390.
- 783 Dugué, L., Merriam, E. P., Heeger, D. J., and Carrasco, M. (2020). Differential impact of  
784 endogenous and exogenous attention on activity in human visual cortex. *Scientific Reports*,  
785 10(1):21274.
- 786 Duyar, A., Denison, R. N., and Carrasco, M. (2023). Exogenous temporal attention varies with  
787 temporal uncertainty. *Journal of Vision*, 23(3):9–9.
- 788 Duyar, A., Ren, S., and Carrasco, M. (2024). When temporal attention interacts with expecta-  
789 tion. *Scientific Reports*, 14(1):4624.
- 790 Fernández, A., Denison, R. N., and Carrasco, M. (2019). Temporal attention improves percep-  
791 tion similarly at foveal and parafoveal locations. *Journal of Vision*, 19(1):12–12.
- 792 Foster, J. J. and Ling, S. (2022). Feature-based attention multiplicatively scales the fMRI-BOLD  
793 contrast-response function. *Journal of Neuroscience*, 42(36):6894–6906.
- 794 Freeman, L. C., Roeder, D., and Mulholland, R. R. (1979). Centrality in social networks: Ii.  
795 experimental results. *Social Networks*, 2(2):119–141.

- 796 Fries, P. (2015). Rhythms for cognition: communication through coherence. *Neuron*,  
797 88(1):220–235.
- 798 Gallager, R. (2003). A minimum delay routing algorithm using distributed computation. *IEEE*  
799 *Transactions on Communications*, 25(1):73–85.
- 800 Gramfort, A., Luessi, M., Larson, E., Engemann, D. A., Strohmeier, D., Brodbeck, C., Goj,  
801 R., Jas, M., Brooks, T., Parkkonen, L., and Hämäläinen, M. S. (2013). MEG and EEG data  
802 analysis with MNE-Python. *Frontiers in Neuroscience*, 7(267):1–13.
- 803 Gregoriou, G. G., Gotts, S. J., Zhou, H., and Desimone, R. (2009). High-frequency, long-range  
804 coupling between prefrontal and visual cortex during attention. *Science*, 324(5931):1207–  
805 1210.
- 806 Hauk, O., Wakeman, D. G., and Henson, R. (2011). Comparison of noise-normalized min-  
807 imum norm estimates for MEG analysis using multiple resolution metrics. *Neuroimage*,  
808 54(3):1966–1974.
- 809 Heart, F. E., Kahn, R. E., Ornstein, S. M., Crowther, W. R., and Walden, D. C. (1970). The  
810 interface message processor for the ARPA computer network. In *Proceedings of the May*  
811 *5-7, 1970, Spring Joint Computer Conference*, pages 551–567.
- 812 Hedrich, T., Pellegrino, G., Kobayashi, E., Lina, J.-M., and Grova, C. (2017). Comparison of the  
813 spatial resolution of source imaging techniques in high-density EEG and MEG. *Neuroimage*,  
814 157:531–544.
- 815 Herweg, N. A., Solomon, E. A., and Kahana, M. J. (2020). Theta oscillations in human memory.  
816 *Trends in Cognitive Sciences*, 24(3):208–227.

- 817 Houck, J. M. and Claus, E. D. (2020). A comparison of automated and manual co-registration  
818 for magnetoencephalography. *PLoS One*, 15(4):e0232100.
- 819 Huang, D., Gao, F., and Chen, Y. (2025). Enhancing visual perception: The independent and  
820 additive effects of temporal and feature-based attention. *Psychonomic Bulletin & Review*,  
821 32(4):1839–1851.
- 822 Huang, S., De Brigard, F., Cabeza, R., and Davis, S. W. (2024). Connectivity analyses for  
823 task-based fMRI. *Physics of Life Reviews*, 49:139–156.
- 824 Isik, L., Meyers, E. M., Leibo, J. Z., and Poggio, T. (2014). The dynamics of invariant object  
825 recognition in the human visual system. *Journal of Neurophysiology*, 111(1):91–102.
- 826 Jing, C., Jin, H., Li, W., Wu, Z., Chen, Y., and Huang, D. (2023). Temporal attention affects  
827 contrast response function by response gain. *Frontiers in Human Neuroscience*, 16:1020260.
- 828 King, J.-R. and Dehaene, S. (2014). Characterizing the dynamics of mental representations: the  
829 temporal generalization method. *Trends in Cognitive Sciences*, 18(4):203–210.
- 830 Klein, A. and Tourville, J. (2012). 101 labeled brain images and a consistent human cortical  
831 labeling protocol. *Frontiers in Neuroscience*, 6:171.
- 832 Kleiner, M., Brainard, D., Pelli, D., Ingling, A., Murray, R., Broussard, C., and Cornelissen, F.  
833 (2007). What is new in psychtoolbox 3. *Perception*, 36(14):1–16.
- 834 Knierim, J. J., Neunuebel, J. P., and Deshmukh, S. S. (2014). Functional correlates of  
835 the lateral and medial entorhinal cortex: objects, path integration and local–global ref-  
836 erence frames. *Philosophical Transactions of the Royal Society B: Biological Sciences*,  
837 369(1635):20130369.

- 838 Kok, P., Jehee, J. F., and De Lange, F. P. (2012). Less is more: expectation sharpens represen-  
839 tations in the primary visual cortex. *Neuron*, 75(2):265–270.
- 840 Kok, P., Mostert, P., and De Lange, F. P. (2017). Prior expectations induce prestimulus sensory  
841 templates. *Proceedings of the National Academy of Sciences*, 114(39):10473–10478.
- 842 Kullback, S. and Leibler, R. A. (1951). On information and sufficiency. *The Annals of Mathe-*  
843 *matical Statistics*, 22(1):79–86.
- 844 Lavenex, P. and Amaral, D. G. (2000). Hippocampal-neocortical interaction: A hierarchy of  
845 associativity. *Hippocampus*, 10(4):420–430.
- 846 Lega, B. C., Jacobs, J., and Kahana, M. (2012). Human hippocampal theta oscillations and the  
847 formation of episodic memories. *Hippocampus*, 22(4):748–761.
- 848 Liu, C., Guo, F., Qian, C., Zhang, Z., Sun, K., Wang, D. J., He, S., and Zhang, P. (2021).  
849 Layer-dependent multiplicative effects of spatial attention on contrast responses in human  
850 early visual cortex. *Progress in Neurobiology*, 207:101897.
- 851 Liu, T., Larsson, J., and Carrasco, M. (2007). Feature-based attention modulates orientation-  
852 selective responses in human visual cortex. *Neuron*, 55(2):313–323.
- 853 Maris, E. and Oostenveld, R. (2007). Nonparametric statistical testing of EEG-and MEG-data.  
854 *Journal of Neuroscience Methods*, 164(1):177–190.
- 855 Maunsell, J. H. and Treue, S. (2006). Feature-based attention in visual cortex. *Trends in Neu-*  
856 *rosciences*, 29(6):317–322.
- 857 McQuillan, J., Richer, I., and Rosen, E. (1980). The new routing algorithm for the arpanet.  
858 *IEEE Transactions on Communications*, 28(5):711–719.

- 859 McQuillan, J. M. and Walden, D. C. (1977). The arpa network design decisions. *Computer*  
860 *Networks (1976)*, 1(5):243–289.
- 861 Meyers, E. M. (2013). The neural decoding toolbox. *Frontiers in Neuroinformatics*, 7:8.
- 862 Mill, R. D. and Cole, M. W. (2025). Dynamically shifting from compositional to conjunctive  
863 brain representations supports cognitive task learning. *Nature Communications*, 16(1):10084.
- 864 Molins, A., Stufflebeam, S. M., Brown, E. N., and Hämäläinen, M. S. (2008). Quantification of  
865 the benefit from integrating MEG and EEG data in minimum  $\ell_2$ -norm estimation. *Neuroim-*  
866 *age*, 42(3):1069–1077.
- 867 Myers, N. E., Stokes, M. G., and Nobre, A. C. (2017). Prioritizing information during working  
868 memory: beyond sustained internal attention. *Trends in Cognitive Sciences*, 21(6):449–461.
- 869 Nobre, A. C. and Van Ede, F. (2023). Attention in flux. *Neuron*, 111(7):971–986.
- 870 Oostenveld, R., Fries, P., Maris, E., and Schoffelen, J.-M. (2011). Fieldtrip: open source soft-  
871 ware for advanced analysis of MEG, EEG, and invasive electrophysiological data. *Computa-*  
872 *tional Intelligence and Neuroscience*, 2011:1–9.
- 873 Palmieri, H. and Carrasco, M. (2024). Task demand mediates the interaction of spatial and  
874 temporal attention. *Scientific Reports*, 14(1):9228.
- 875 Pantazis, D., Fang, M., Qin, S., Mohsenzadeh, Y., Li, Q., and Cichy, R. M. (2018). Decoding  
876 the orientation of contrast edges from MEG evoked and induced responses. *NeuroImage*,  
877 180:267–279.
- 878 Pedregosa, F., Varoquaux, G., Gramfort, A., Michel, V., Thirion, B., Grisel, O., Blondel, M.,  
879 Prettenhofer, P., Weiss, R., Dubourg, V., Vanderplas, J., Passos, A., Cournapeau, D., Brucher,

- 880 M., Perrot, M., and Duchesnay, E. (2011). Scikit-learn: Machine learning in Python. *Journal*  
881 *of Machine Learning Research*, 12:2825–2830.
- 882 Pelli, D. G. and Vision, S. (1997). The videotoolbox software for visual psychophysics: Trans-  
883 forming numbers into movies. *Spatial Vision*, 10:437–442.
- 884 Ranganath, C. and Ritchey, M. (2012). Two cortical systems for memory-guided behaviour.  
885 *Nature Reviews neuroscience*, 13(10):713–726.
- 886 Saalmann, Y. B., Pigarev, I. N., and Vidyasagar, T. R. (2007). Neural mechanisms of visual  
887 attention: how top-down feedback highlights relevant locations. *Science*, 316(5831):1612–  
888 1615.
- 889 Saalmann, Y. B., Pinsk, M. A., Wang, L., Li, X., and Kastner, S. (2012). The pulvinar regu-  
890 lates information transmission between cortical areas based on attention demands. *Science*,  
891 337(6095):753–756.
- 892 Salinas, E. and Sejnowski, T. J. (2001). Correlated neuronal activity and the flow of neural  
893 information. *Nature Reviews Neuroscience*, 2(8):539–550.
- 894 Siegel, M., Buschman, T. J., and Miller, E. K. (2015). Cortical information flow during flexible  
895 sensorimotor decisions. *Science*, 348(6241):1352–1355.
- 896 Stokes, M. G., Wolff, M. J., and Spaak, E. (2015). Decoding rich spatial information with high  
897 temporal resolution. *Trends in Cognitive Sciences*, 19(11):636–638.
- 898 Tian, K. J., Motzer, J. A., and Denison, R. N. (2026). Voluntary temporal atten-  
899 tion improves perception even in the absence of temporal competition. *bioRxiv*.  
900 doi:10.64898/2026.02.11.705419.

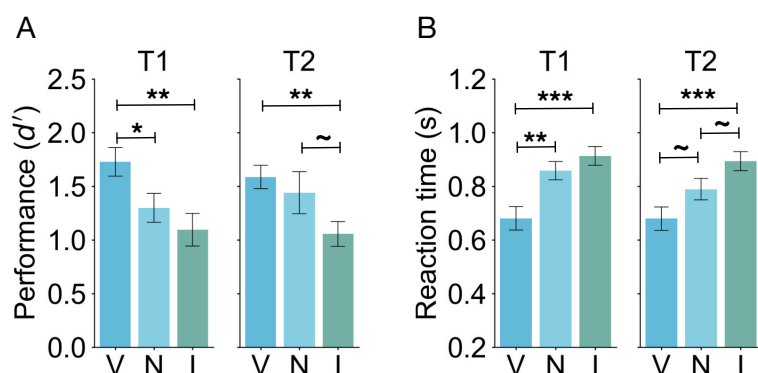
- 901 Todd, J. J. and Marois, R. (2004). Capacity limit of visual short-term memory in human poste-  
902 rior parietal cortex. *Nature*, 428(6984):751–754.
- 903 Van Ede, F., Chekroud, S. R., Stokes, M. G., and Nobre, A. C. (2018). Decoding the influence  
904 of anticipatory states on visual perception in the presence of temporal distractors. *Nature*  
905 *Communications*, 9(1):1449.
- 906 van Es, D. M., Theeuwes, J., and Knapen, T. (2018). Spatial sampling in human visual cortex  
907 is modulated by both spatial and feature-based attention. *eLife*, 7:e36928.
- 908 Váša, F. and Mišić, B. (2022). Null models in network neuroscience. *Nature Reviews Neuro-*  
909 *science*, 23(8):493–504.
- 910 Wallis, G., Stokes, M., Cousijn, H., Woolrich, M., and Nobre, A. C. (2015). Frontoparietal and  
911 cingulo-opercular networks play dissociable roles in control of working memory. *Journal of*  
912 *Cognitive Neuroscience*, 27(10):2019–2034.
- 913 Wang, L., Schoot, L., Brothers, T., Alexander, E., Warnke, L., Kim, M., Khan, S., Hämäläinen,  
914 M., and Kuperberg, G. R. (2023). Predictive coding across the left fronto-temporal hierarchy  
915 during language comprehension. *Cerebral Cortex*, 33(8):4478–4497.
- 916 Wardle, S. G., Kriegeskorte, N., Grootswagers, T., Khaligh-Razavi, S.-M., and Carlson, T. A.  
917 (2016). Perceptual similarity of visual patterns predicts dynamic neural activation patterns  
918 measured with MEG. *Neuroimage*, 132:59–70.
- 919 Wilming, N., König, P., König, S., and Buffalo, E. A. (2018). Entorhinal cortex receptive fields  
920 are modulated by spatial attention, even without movement. *eLife*, 7:e31745.
- 921 Womelsdorf, T., Schoffelen, J.-M., Oostenveld, R., Singer, W., Desimone, R., Engel, A. K.,

- 922 and Fries, P. (2007). Modulation of neuronal interactions through neuronal synchronization.  
923 *Science*, 316(5831):1609–1612.
- 924 Xu, Y. (2018a). The posterior parietal cortex in adaptive visual processing. *Trends in Neuro-*  
925 *sciences*, 41(11):806–822.
- 926 Xu, Y. (2018b). A tale of two visual systems: Invariant and adaptive visual information repre-  
927 sentations in the primate brain. *Annual Review of Vision Science*, 4(1):311–336.
- 928 Xu, Y. (2024). The human posterior parietal cortices orthogonalize the representation of dif-  
929 ferent streams of information concurrently coded in visual working memory. *PLoS Biology*,  
930 22(11):e3002915.
- 931 Zhu, J., Tian, K. J., Carrasco, M., and Denison, R. N. (2024). Temporal attention amplifies  
932 stimulus information in fronto-cingulate cortex at an intermediate processing stage. *PNAS*  
933 *Nexus*, 3(12):pgae535.

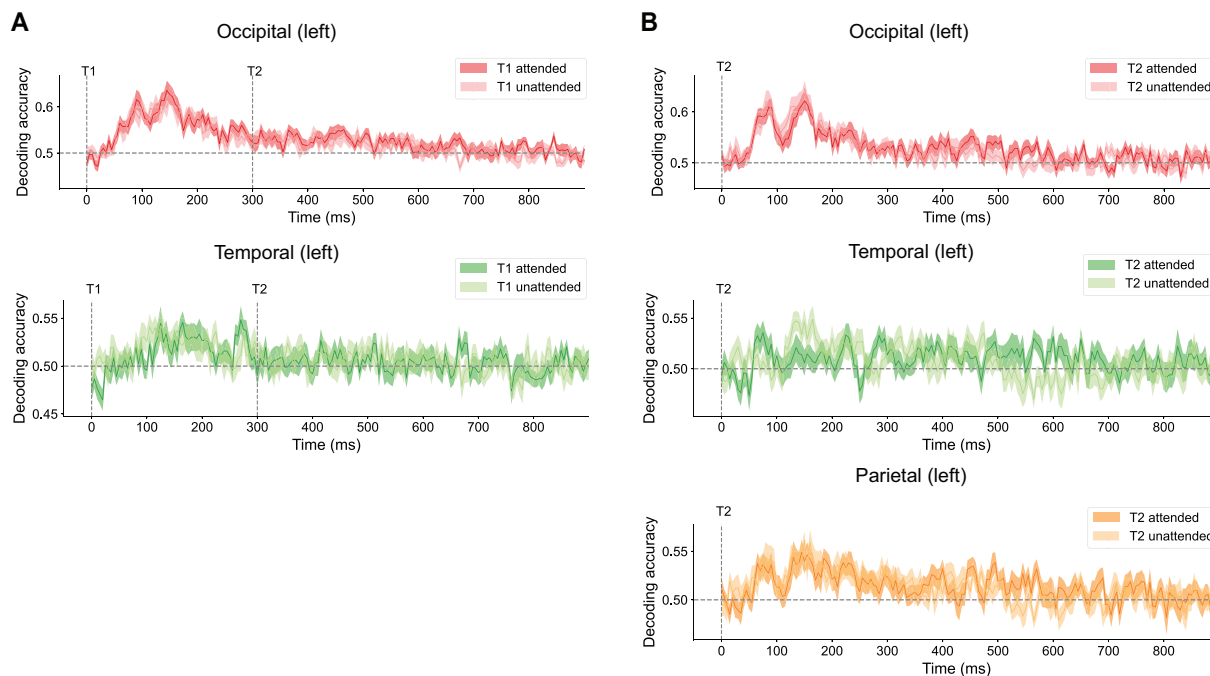
934 **Supplementary Figures and Tables**

**Supplementary Table 1.** Node number for 68 atlas-based ROIs

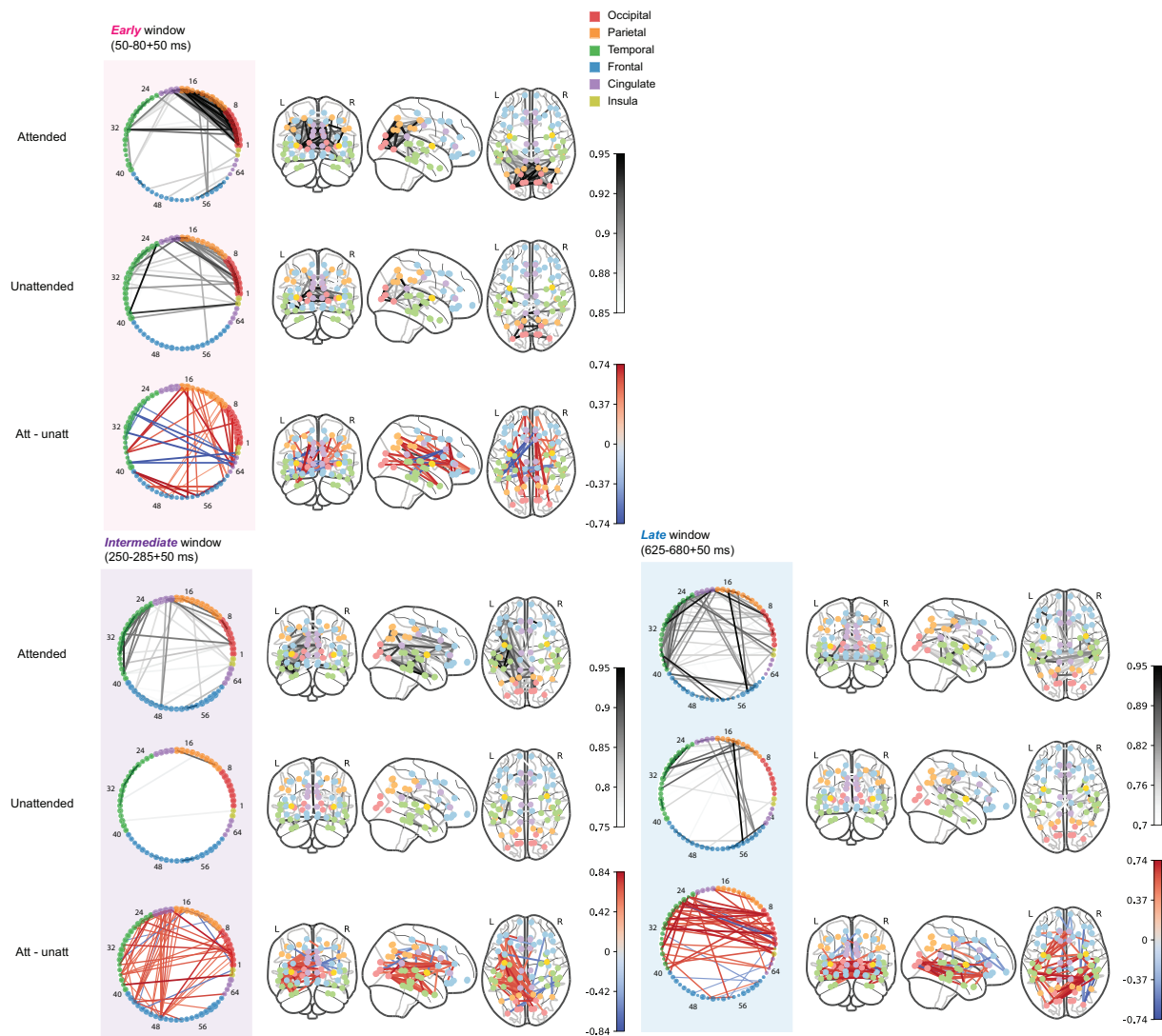
ROI#	Occipital	ROI#	Parietal	ROI#	Temporal
1	left lateral occipital	9	left superior parietal	19	left superior temporal
2	right lateral occipital	10	right superior parietal	20	right superior temporal
3	left lingual	11	left inferior parietal	21	left middle temporal
4	right lingual	12	right inferior parietal	22	right middle temporal
5	left cuneus	13	left supramarginal	23	left inferior temporal
6	right cuneus	14	right supramarginal	24	right inferior temporal
7	left pericalcarine	15	left postcentral	25	left bankssts
8	right pericalcarine	16	right postcentral	26	right bankssts
		17	left precuneus	27	left fusiform
		18	right precuneus	28	right fusiform
ROI#	Temporal	ROI#	Frontal	ROI#	Frontal
29	left transverse temporal	37	left superior frontal	45	left pars opercularis
30	right transverse temporal	38	right superior frontal	46	right pars opercularis
31	left entorhinal	39	left rostral middle frontal	47	left pars orbitalis
32	right entorhinal	40	right rostral middle frontal	48	right pars orbitalis
33	left temporal pole	41	left caudal middle frontal	49	left lateral orbitofrontal
34	right temporal pole	42	right caudal middle frontal	50	right lateral orbitofrontal
35	left parahippocampal	43	left pars triangularis	51	left medial orbitofrontal
36	right parahippocampal	44	right pars triangularis	52	right medial orbitofrontal
ROI#	Frontal	ROI#	Cingulate	ROI#	Insula
53	left precentral	59	left isthmus cingulate	67	left insula
54	right precentral	60	right isthmus cingulate	68	right insula
55	left paracentral	61	left posterior cingulate		
56	right paracentral	62	right posterior cingulate		
57	left frontal pole	63	left rostral anterior cingulate		
58	right frontal pole	64	right rostral anterior cingulate		
		65	left caudal anterior cingulate		
		66	right caudal anterior cingulate		



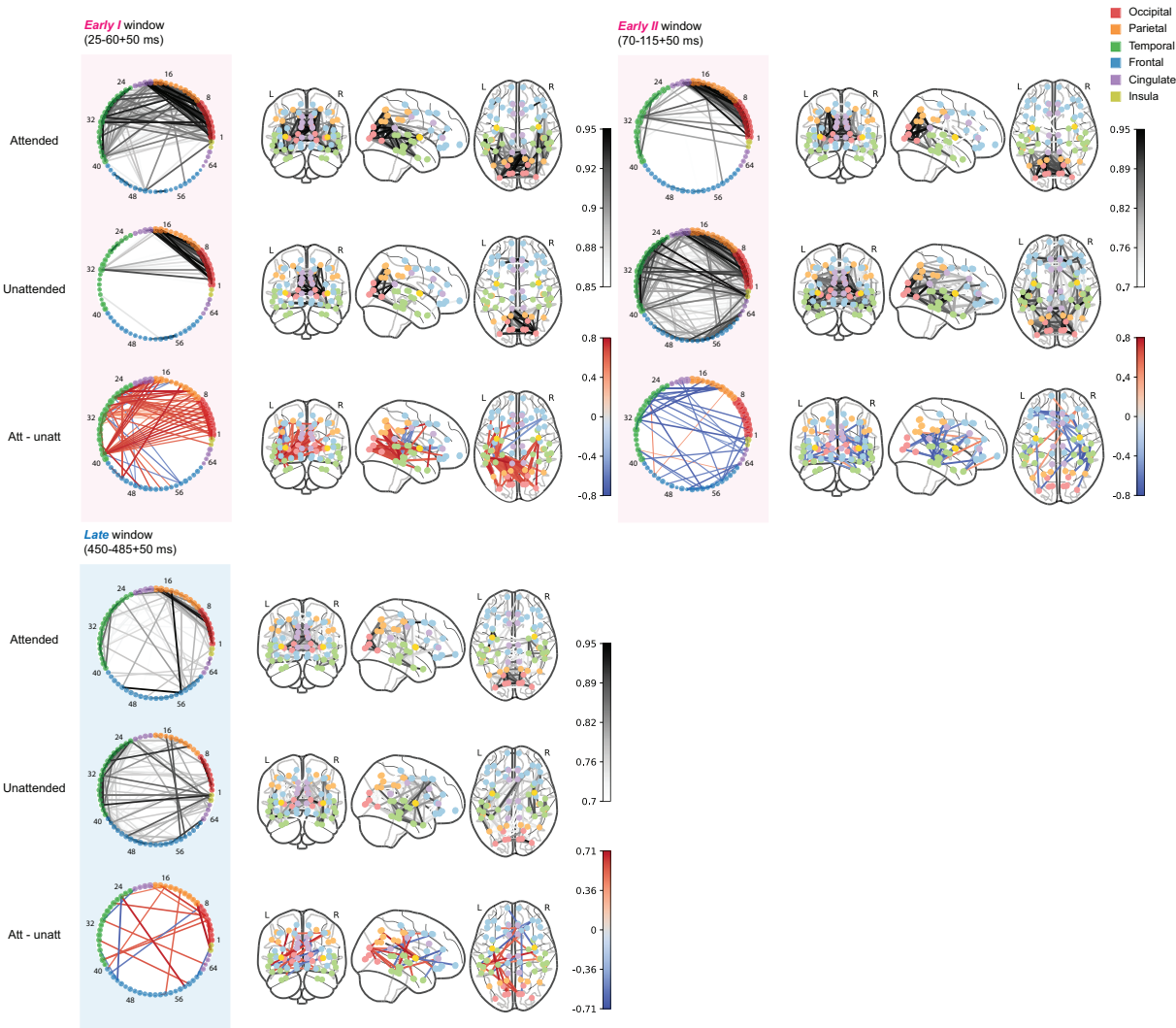
**Supplementary Figure 1.** Behavioral results including the neutral condition. Perceptual sensitivity was impaired in the neutral condition (when the temporal precue was uninformative), relative to the valid condition for T1. This result confirms that observers could not fully process both stimuli and instead relied on attention to select the more relevant stimulus in the sequence. Such behavioral benefits are consistent with previous studies using the two-target temporal cueing task (Denison et al., 2017, 2021; Fernández et al., 2019; Duyar et al., 2024), indicating that this task reliably elicits temporal attentional selection. **(A)** Tilt discrimination (sensitivity) and **(B)** reaction time for each target (T1, T2) and validity condition (V = valid, N = neutral, I = invalid). Error bars indicate  $\pm 1$  SEM.  $\sim p < 0.1$ ,  $* p < 0.05$ ,  $** p < 0.01$ ;  $*** p < 0.001$ .



**Supplementary Figure 2.** Decoding accuracy for target attended vs target unattended in different lobes. **(A)** Decoding accuracies for T1 in lobes that show enhancement of closeness centrality in **Figure 3**. **(B)** Decoding accuracies for T2 in lobes that show enhancement of closeness centrality in **Figure 4**.



**Supplementary Figure 3.** Visualization for averaged dynamic informational connectivity networks for T1 at different critical time windows. For each time window, the network is shown as a chord diagram in which each node represents an ROI; corresponding coronal, sagittal, and axial views are shown from left to right. The visualization of target attended networks is on the first row, and target unattended networks are on the second row. The darker the edges between the nodes, the stronger the connectivity is between them. The third row shows the difference in informational connectivity between attended and unattended conditions. The presented edges are  $p < 0.01$  compared to a shuffled null distribution. Edges with higher values are shown in red, indicating greater connectivity during the attended than the unattended condition.



**Supplementary Figure 4.** Visualization for averaged dynamic informational connectivity networks for T2 at different critical time windows. For each time window, the network is shown as a chord diagram in which each node represents an ROI; corresponding coronal, sagittal, and axial views are shown from left to right. The visualization of target attended networks is on the first row, and target unattended networks are on the second row. The darker the edges between the nodes, the stronger the connectivity is between them. The third row shows the difference in informational connectivity between attended and unattended conditions. The presented edges are  $p < 0.01$  compared to a shuffled null distribution. Edges with higher values are shown in red, indicating greater connectivity during the attended than the unattended condition.